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DOI: 10.3109/17435390.2014.992487

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Document Version
Publisher's PDF, also known as Version of record

Citation for published version (Harvard):

Link to publication on Research at Birmingham portal

Publisher Rights Statement:
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To cite this article: Zofi McKenzie, Michaela Kendall, Rose-Marie Mackay, Harry Whitwell, Christine Elgy, Ping Ding, Sumeet Mahajan, Cliff Morgan, Mark Griffiths, Howard Clark & Jens Madsen (2015) Surfactant protein A (SP-A) inhibits agglomeration and macrophage uptake of toxic amine modified nanoparticles, Nanotoxicology, 9:8, 952-962, DOI: 10.3109/17435390.2014.992487

To link to this article: http://dx.doi.org/10.3109/17435390.2014.992487
Surfactant protein A (SP-A) inhibits agglomeration and macrophage uptake of toxic amine modified nanoparticles

Zofi McKenzie\textsuperscript{1*}, Michaela Kendall\textsuperscript{1,2*}, Rose-Marie Mackay\textsuperscript{1}, Harry Whitwell\textsuperscript{1}, Christine Elgy\textsuperscript{2}, Ping Ding\textsuperscript{3}, Sumeet Mahajan\textsuperscript{4,5}, Cliff Morgan\textsuperscript{6}, Mark Griffiths\textsuperscript{6}, Howard Clark\textsuperscript{1,4,7}, and Jens Madsen\textsuperscript{1,4,7}

\textsuperscript{1}Department of Child Health, Clinical and Experimental Sciences, Faculty of Medicine, Southampton General Hospital, University of Southampton, Southampton, UK, \textsuperscript{2}School of Geography, Earth and Environmental Sciences, University of Birmingham, Birmingham, UK, \textsuperscript{3}Facility for Environmental Nanoscience Analysis and Characterisation (FENAC), School of Metallurgy and Materials, University of Birmingham, Birmingham, UK, \textsuperscript{4}Institute for Life Sciences, University of Southampton, Highfield, Southampton, UK, \textsuperscript{5}Department of Chemistry, University of Southampton, Highfield, Southampton, UK, \textsuperscript{6}Leukocyte Biology, Royal Brompton Campus, Imperial College London, London, UK, and \textsuperscript{7}National Institute for Health Research, Southampton Respiratory Biomedical Research Unit, Southampton Centre for Biomedical Research, University Hospital Southampton NHS Foundation Trust, Southampton, UK

Abstract

The lung provides the main route for nanomaterial exposure. Surfactant protein A (SP-A) is an important respiratory innate immune molecule with the ability to bind or opsonise pathogens to enhance phagocytic removal from the airways. We hypothesised that SP-A, like surfactant protein D, may interact with inhaled nanoparticulates, and that this interaction will be affected by nanoparticle (NP) surface characteristics. In this study, we characterise the interaction of SP-A with unmodified (U-PS) and amine-modified (A-PS) polystyrene particles of varying size and zeta potential using dynamic light scatter analysis. SP-A associated with both 100 nm U-PS and A-PS in a calcium-independent manner. SP-A induced significant calcium-dependent agglomeration of 100 nm U-PS NPs but resulted in calcium-independent inhibition of A-PS self-agglomeration. SP-A enhanced uptake of 100 nm U-PS into macrophage-like RAW264.7 cells in a dose-dependent manner but in contrast inhibited A-PS uptake. Reduced association of A-PS particles in RAW264.7 cells following pre-incubation of SP-A was also observed with coherent anti-Stokes Raman spectroscopy. Consistent with these findings, alveolar macrophages (AMs) from SP-A\textsuperscript{−/−} mice were more efficient at uptake of 100 nm A-PS compared with wild type C57Bl/6 mice. No difference in uptake was observed with 500 nm U-PS or A-PS particles. Pre-incubation with SP-A resulted in a significant decrease in uptake of 100 nm A-PS in macrophages isolated from both groups of mice. In contrast, increased uptake by AMs of U-PS was observed after pre-incubation with SP-A. Thus we have demonstrated that SP-A promotes uptake of non-toxic U-PS particles but inhibits the clearance of potentially toxic A-PS particles by blocking uptake into macrophages.

Introduction

The ability of nanotechnology to produce engineered nanoparticles (NPs) of various shapes and materials has opened up new applications in areas such as medicine, engineering, electronics, textiles and cosmetics. The number of consumer products containing NPs is rapidly increasing and is now counted in thousands (Nanotechnologies, 2014). This reflects the unique and diverse properties of nanomaterials, which can be very different from the bulk material due, in part, to their enhanced surface to mass ratio (Oberdörster et al., 2005a).

Exposure to nanomaterials is not a new phenomenon. Throughout evolution, humans have been exposed to nanosized particles from both biogenic and anthropogenic sources. However, human lung exposures have risen dramatically due to anthropogenic emission from diesel engines, power stations and engineering processes optimised for manufacturing nanoscale materials (Oberdörster et al., 2005b). Due to the small size of nanomaterials, they are often airborne and have the capability of reaching the alveolar compartment of the lungs (Oberdörster et al., 2002, 2005b). Once inside the airways, the NPs can be adsorbed onto the mucusal surface in the upper airways and into surfactant lining the lower airways. A nano-bio corona of biological molecules then forms on the NP surface, which can in turn influence the clearance, bioavailability and potential toxicity of the NPs (recently reviewed in Kendall & Holgate (2012)).

Pulmonary surfactant is a multi-layered lipoprotein substance, comprising approximately 90% lipids and 10% protein, and lines...
the alveolar epithelium at the air liquid interface. Pulmonary surfactant performs two vital functions in the lung; reducing alveolar surface tension and protecting the lung from microbial infection (reviewed in Périz-Gil (2008)). Surfactant protein A (SP-A) and its sister protein surfactant protein D (SP-D) are both hydrophilic proteins found in surfactant belonging to the calcium-dependent (C-type) lectin sub-family known as “collectins” (collagenous lectins). Collectins are oligomeric proteins made up of trimeric units. The trimeric units are composed of three monomers, each with its own carbohydrate recognition domain (CRD) containing the lectin activity (Figure S1). The trimeric units are characterised by four structural domains: an amino terminus (where the oligomerisation between trimeric units take place), a collagenous domain, a neck region and the CRD region. Six of these trimeric units oligomerise to form octadecamers, the native form of SP-A (Figure S1). As SP-A has a bend in the collagenous region, the quaternary structure has been described as a “bunch of tulips” similar to the complement C1q molecule (Voss et al., 1988). Four trimeric units come together to form SP-D in the shape of a cross (Figure S1). SP-A is the most abundant of the two proteins with approximately 10 times more SP-A in surfactant than SP-D (Pastva et al., 2007). The pulmonary collectins, SP-A and SP-D, play an important role in the innate immune defence of the lung; they are pattern recognition molecules and are able to protect the lung from infection through a variety of mechanisms. They recognise and bind specific carbohydrate moieties on the surface of micro-organisms via the CRD and can facilitate microbial clearance through agglutination and opsonisation (reviewed in Pastva et al. (2007)). They also promote uptake and clearance of dead and dying apoptotic cells in the airway and bind to cell-surface exposed and free DNA debris (Clark et al., 2002; Palaniyar et al., 2007). They also promote uptake and clearance of dead and dying cells. The pulmonary collectins, SP-A and SP-D, play an important role in the innate immune defence of the lung; they are pattern recognition molecules and are able to protect the lung from infection through a variety of mechanisms. They recognise and bind specific carbohydrate moieties on the surface of micro-organisms via the CRD and can facilitate microbial clearance through agglutination and opsonisation (reviewed in Pastva et al. (2007)). They also promote uptake and clearance of dead and dying apoptotic cells in the airway and bind to cell-surface exposed and free DNA debris (Clark et al., 2002; Palaniyar et al., 2007). They also promote uptake and clearance of dead and dying cells.

In vitro and in vivo studies with mice deficient for SP-A (SP-A / / mice) have shown that SP-A is important for the phagocytosis and clearance of both bacteria and viruses from the lung (LeVine et al., 1997, 1998, 1999a,b, 2002; Li et al., 2002). Recent studies have suggested that SP-A and SP-D also play a role in the clearance of non-infectious particulate matter in the lung (Kendall et al., 2013; Ruge et al., 2011, 2012).

We have previously characterised the interaction of SP-D with various NPs including unmodified (U-PS) and amine (A-PS) surface-modified polystyrene particles (Kendall et al., 2013). SP-D co-localised to 200 nm A-PS NPs in A549 epithelium cells in vitro (Kendall et al., 2013). Furthermore, alveolar macrophages (AMs) from wild type (WT) C57Bl/6 mice showed enhanced uptake of both 100 nm and 500 nm U-PS and A-PS particles compared with AMs isolated from mice deficient in SP-D (SP-D / / mice) (Kendall et al., 2013). Addition of exogenous SP-D to AMs from SP-D / / mice enhanced the percentage of AMs taking up 100 nm A-PS (Kendall et al., 2013). Both SP-A and SP-D have been found to bind to carbon nanotubes (Salvador-Morales et al., 2007). The binding was calcium-dependent and was variable between batches of nanotubes indicating that the binding was mediated by surface impurities or chemical modifications of the nanotubes (Salvador-Morales et al., 2007). Differential interaction of SP-A was also observed with metal oxide NPs, including titanium oxide and cerium oxide particles, where differences were seen with different surface-modified particles derived from the same bulk-material highlighting the importance of the particle size, surface charge and chemistry (Schulze et al., 2011). SP-A has also been found to bind to certain surface-modified magnetic NPs (Ruge et al., 2011). It was shown that SP-A specifically interacted with magnetic NPs modified with starch, carboxymethylxanthan, chitosan, poly-maleic-oleic acid and phosphatidylcholine compared with bovine serum albumin (BSA) (Ruge et al., 2011). SP-A also enhanced the association of the surface-modified magnetic particles to AMs, except for starch, when compared with BSA. Furthermore, SP-A increased the uptake of phosphatidylcholine NPs into AMs, whereas the presence of BSA resulted in a decrease in particles taken up by the cells (Ruge et al., 2011). SP-A was also found to facilitate the uptake of aggregated NP-sized tacrolimus complexes (an immunosuppressive agent) into human macrophage-like U937 cells.

In this study, we characterise the interaction of SP-A with polystyrene NPs with well-defined different surface characteristics and size. As in previous studies with SP-D, we focused on U-PS and A-PS at 100, 200 and 500 nm. We characterised the effect of SP-A on uptake of NPs in the murine macrophage cell line, RAW264.7, before extending the results into primary AMs isolated from SP-A-deficient mice and C57Bl/6 wild type control mice. The effects of interaction of SP-A and NPs are distinct from our previous report for SP-D.

Materials and methods

Nanoparticles

Polystyrene particles with and without surface modification with sizes of 100 nm, 200 nm and 500 nm were purchased (Polysciences Inc, Northampton, UK or Sigma-Aldrich, Dorset, UK). The particles were unmodified polystyrene (U-PS), amine-modified polystyrene (A-PS) and carboxylate-modified polystyrene (C-PS). Fluorescent green 100 nm U-PS and fluorescent orange 100 nm A-PS were purchased from Polysciences and Sigma-Aldrich, respectively.

SP-A purification

Human bronchoalveolar lavage (BAL) was obtained from patients with written informed consent undergoing lung washings for therapeutic purposes including pulmonary alveolar proteinosis. The procedure was approved by the London National Health Service Research Ethics Committee (NRES reference 10/H0504/9). Native human SP-A was purified from the SP-A-rich BAL pellet either by gel chromatography or butanol extraction as described previously (Suwabe et al., 1996; Wright et al., 1987). The purity of SP-A was verified by sodium dodecyl sulphate polyacrylamide gel electrophoresis (SDS-PAGE), Western blotting and N-terminal sequencing. The purified SP-A protein was diluted with nanopure water or Tris-buffered saline (TBS) with 2–5 mM calcium before mixing with particles.

Characterisation of the NP and SP-A interaction by dynamic light scatter analysis and zeta potential

The interaction between SP-A and NPs was characterised by dynamic light scatter (DLS; HPPS and Zetasizer Nano ZS, Malvern Instruments, Worcestershire, UK) and zeta potential (ZP; Zetasizer Nano ZS, Malvern Instruments). This was initially performed in nano pure water as described previously (Kendall et al., 2013). The DLS and ZP analyses were also performed in TBS and serum-free (SF) RPMI-1640 medium without phenol red (Gibco, Life Technologies, UK). In these experiments, A-PS or U-PS particles were suspended in TBS with 5 mM calcium at a concentration of 12.5 cm2/mL. These particles were diluted with equal volumes of protein (SP-A or BSA) suspended in

DOI: 10.3109/17435390.2014.992487
TBS + calcium at 50 μg/mL. The size and ZPs of these suspensions were measured immediately before (T-2) and after (T0) the addition of protein. The particle suspensions were then incubated at 37 °C for 48 min, the size and ZP were then measured before (T48) and after (T60) the addition of SF RPMI. This yielded a TBS/RPMI ratio of 2:3 and final concentrations of proteins and particles of 10 μg/mL and 2.5 cm²/mL, respectively. The size and ZP of the suspensions were measured again following incubation for a further two hours at 37 °C (T180). All measurements were conducted at 37 °C using reusable or disposable capillary cells (Malvern Instruments).

RAW cells

RAW264.7 cells are a mouse macrophage-like cell line established from murine tumours induced with Abelson leukaemia virus (Raschke et al., 1978). Cells were routinely grown in RPMI-1640 (Gibco) supplemented with 1% L-glutamine (Gibco), 1% penicillin/streptomycin (Gibco) and 10% heat-inactivated foetal calf serum (Sigma-Aldrich) at 37 °C in a humidified atmosphere with 5% CO₂. The semi-adherent cell line was routinely sub-cultured using a cell scraper every third day.

Uptake of unlabelled A-PS NPs

Uptake of unlabelled A-PS NPs

RAW264.7 cells were scrapped and plated in six-well plates on sterile cover slips with 500 000 cells/well. The cells were allowed to adhere for 24 hours, and then the cells were incubated with 5 μL of NPs (in general 10¹³ NPs/mL corresponding to 5 × 10¹⁰ NP/well) in a total volume of 1 mL SF RPMI medium for two hours. The cells were washed carefully with phosphate-buffered saline (PBS) twice and then fixed in 1% paraformaldehyde in PBS for one hour at room temperature. The cover slips, with attached cells, were mounted on a glass side upside down and the edges sealed with clear nail polish. The slides were then analysed using Coherent anti-Stokes Raman scattering (CARS).

Uptake of fluorescent A-PS and U-PS particles in RAW cells

Aliquots of 100 nm fluorescent orange A-PS or fluorescent green U-PS particles were mixed with SP-A in TBS containing 5 mM calcium to yield concentrations of 9.4 cm²/mL particles and 25 μg/mL proteins. Particle–protein suspensions were incubated for one hour at 37 °C in 96-well round bottom plates. RAW264.7 cells were washed three times in SF RPMI and dissociated from culture flasks using a cell scraper. Cells were suspended in SF RPMI at a concentration of 1.67 × 10⁶ cells/mL, and 30 μL aliquots were added to each well yielding a final particle concentration of 3.75 cm²/mL and a TBS/RPMI ratio of 2:3. The cells were incubated for one hour at 37 °C in a humidified atmosphere. The cells were washed once in 1 mL PBS and centrifuged at 400 g for 10 min to remove excess particles. The cells were resuspended in 40 μL PBS and kept on ice prior to analysis. Trypan blue was added to the cells immediately before the analysis of 5000 cells per sample using flow cytometry (BD FACS Aria, BD Biosciences, Oxford, UK).

CARS analysis

CARS microscopy is a label-free chemical imaging technique, which generates contrast using molecular vibrations, which are specific to an individual molecule (Patel et al., 2013). A home-built CARS setup comprising of a Chameleon (Coherent) and Compact OPO (APE Berlin) coupled to an inverted Nikon Ti-U 2000 microscope (Nikon, Kingston upon Thames, UK) was used to acquire images. The beams were temporally overlapped using a delay stage and combined to form a spatially overlapped collinear beam. The pump beam was set to 835 nm, and the Stokes beam from the OPO was tuned to target the Raman frequency of 2850 cm⁻¹ to target the CH₂ stretching band. Due to the higher concentration of CH₂ bonds in polystyrene beads and the fact that CARS has a quadratic dependence on the number of oscillators, the PS beads offer high contrast to enable qualitative and quantitative analysis. Amine-modification of the surface of a polystyrene bead will not affect the bulk of the –CH₂ CARS signal (at 2850 cm⁻¹) from the 200 and 500 nm beads used in this work and changes, if any, are well within the spectral resolution of the system.

A series of images was taken for every time point and each individual cell sample. Dwell times of 30 μs were usually chosen, and an area of 30 μm × 30 μm scanned at 1024 × 1024 pixels to generate a highly resolved image. Images were acquired with a 40 × (NA: 1.2) water-immersion objective for each separate treatment. In separate experiments to characterise the spatial (lateral) resolution of the CARS microscope, particles of various sizes (100–1000 nm) were imaged. It was found that 200 nm sized PS particles were resolvable and hence, the quantitative analysis based on CARS was carried out >200 nm particles. At the above target vibrational frequency of 2850 cm⁻¹, the PS particles showed up as highly CARS-active areas, which were quantified using a code written in MATLAB (MathWorks, Cambridge, UK). The number of pixels with intensities exceeding a certain threshold (defined by the background) was counted. This area contributing to the signal is related directly to the number of NPs due to the nature of the CARS signal generation process (multiphoton and hence, inherently confined to the focal plane), and the images presented in this work are 2D rather than 3D projections/stacks. This number corresponding to the bright areas was compared with the overall cell area in pixels to obtain a ratio of NP over cell area.

Mouse BAL and isolation of AMs

Wild type (WT) C57Bl/6 mice and SP-A-deficient mice (SP-A⁻/⁻; Li et al., 2002), back-crossed at least 10 times onto the C57Bl/6 mouse background, were housed in specific pathogen-free housing at the Biomedical Research Facility at the University of Southampton. Mice received sterile rodent chow and water ad libitum with a 12-hour light and dark cycle. All animal procedures were approved by university local animal ethics committee and the Home Office, UK. The mice were sacrificed by CO₂ asphyxiation prior to cannulation of the trachea with a fine bore cannula. The BAL was performed by instillation and withdrawal of 3 × 1 mL of PBS with 0.5 mM EDTA, which was subsequently pooled. Cells were pelleted by centrifugation at 300 g for 10 min. The cell pellet was re-suspended in SF RPMI. Differential cell counts on cytospin preparations after staining with Diff-Quick (Scientific Products, McGaw Park, IL) confirmed that more than 95% of the cells isolated this way were AMs.

AM uptake of fluorescent microspheres

The NPs used in the ex vivo experiments were either 100 nm or 500 nm U-PS (Sigma-Aldrich) or A-PS (Sigma-Aldrich) and were labelled with green fluorescent dye (fluorescein isothiocyanate (FITC), Sigma-Aldrich) dissolved in carbonate buffer (Sigma-Aldrich) at pH 9.6 at a concentration of 1 mg/mL. The FITC was then diluted 1:10 in nanopure water containing the NPs and incubated at room temperature for one hour with rotation. The NPs were centrifuged for 10 min at 20 937 g and washed twice with nanopure water. We have previously shown that the coupling of FITC to the NPs by this methodology only provides minimal leaching at pH 7.4 and 4.0, to mimic the conditions of the
extracellular and endosomal environments, respectively (Kendall et al., 2013). AMs were isolated from C57Bl/6 and SP-A−/− mice as described above, the cells were washed and then incubated with NPs (1:5; 25 000 cells:125 000 NPs), after 5 min sonication, at 37 °C for 30 min. The cells were centrifuged at 300 g for 10 min and washed three times with RPMI (Gibco) to remove excess beads and re-suspended in cytofix (BD Biosciences) containing 0.2% trypan blue to quench extracellular fluorescence as previously described (Hartshorn et al., 1994). The fixed cells were then analysed by fluorescence-activated cell sorting (FACS).

### Results

We have previously measured the size distributions and ZP of a range of similarly sized polystyrene particles (A-PS, C-PS and U-PS), silicone particles (200 V and R816) and carbon black particles (CB400R) in water over time with the addition of purified human SP-D (Kendall et al., 2013). These results showed that SP-D interacted differently with these particles. In this study, we present the interaction of A-PS and U-PS particles with purified human SP-A.

The size distribution of purified human SP-A in water was measured by light intensity and number. The SP-A preparation was polydispersed with two peaks between 10 and 500 nm. A few macromolecules were also evident in this preparation with a small peak around 4500 nm. The majority of the human SP-A, measured by number of particles, showed a median of 30 nm in size (Figure S2). The ZP of SP-A alone in water was −11.8 mV.

In order to fully characterise the effect of SP-A on particle size and ZP, these measurements were taken in nanopure water and the media used for cell experiments (i.e. TBS/RPMI). First, we examined the hydrodynamic size and ZPs of A-PS and U-PS particles in nanopure water without calcium with and without the addition of SP-A (Table S1). In nanopure water, A-PS particles had a strong positive (+60 mV) ZP, which became negative with the addition of SP-A (−22.8 mV). U-PS particles had a ZP of −38.5 mV, which moved closer to zero following the addition of SP-A (−18.7 mV). The z average increased for both A-PS (49.1%) and U-PS (14.3%) particles when incubated with SP-A for 1440 min (Table S1).

The extent of the increase in the z average for 100 nm U-PS particles when incubated with SP-A for 24 hours is indicative of the formation of a protein corona rather than particle agglomeration. Calcium is essential for the lectin activity of SP-A as the ion is involved in the coordination of several of the amino acid residues involved in binding to carbohydrates (Head et al., 2003). We therefore investigated the effect of calcium concentration on the agglomeration rate of 100 nm U-PS particles within a range of 0–2 mM of calcium to elucidate if the CRD in SP-A could be involved in agglomeration. The results showed that the agglomeration rate of U-PS depended on the calcium concentration with the addition of 2 mM of calcium required for SP-A-mediated agglomeration to occur (Figure S3B). When the calcium concentration was 1 mM or lower, agglomeration of U-PS particles in the presence of SP-A was not observed. In the presence of 2 mM calcium, SP-A agglomerated the U-PS particles within 10 min, and the agglomerates increased in size over time (Figure S3C). Based on these results, a minimum concentration of 2 mM CaCl₂ was used in the following experiments.

In order to maintain the calcium concentration above 2 mM at all stages of the in vitro cellular experiments, the particles were pre-incubated with SP-A in TBS containing 5 mM calcium before the addition of cells suspended in SF RPMI media. The proportion of TBS to RPMI used in the experiments (2:3) was pre-determined not to cause precipitation of calcium – which occurred following the addition of 2 mM calcium directly to RPMI. The size and ZPs were measured in TBS or TBS/RPMI at various time points (T-2 to T180). These results are listed in Table 1 and Figures 1 and 2. The time points chosen reflect the incubation periods for the in vitro cellular experiments. Size and ZP were measured in TBS + Ca immediately before (T-2) and after (T0) the addition of protein. The particle–protein suspensions were incubated at 37 °C and the size distributions and ZP measured before (T48) and after (T60) the addition of RPMI. This incubation period reflected the pre-incubation of particles and proteins before the addition of cells. The particle suspensions were incubated again for a further two hours to reflect the incubation period with the cells (T180).

Interestingly, the incubation of A-PS particles in TBS/RPMI (T60) resulted in the self agglomeration of the particles at physiological temperatures (i.e. 37 °C); pre-incubation with SP-A resulted in a reduction in the A-PS particle self agglomeration at this temperature. BSA also inhibited this self agglomeration (Figure 1A and Table 1). The particle size distributions show that SP-A reversed the self agglomeration of A-PS particles over time (Figure 1B). However, this did not seem to be the case when examining the Z-average of the particles (Table 1). This may be related to the high polydispersity of the samples and the presence of a few large agglomerates skewing the z average. The incubation of SP-A with U-PS particles for 60 min at 37 °C greatly enhanced the particle size (Figure 1C). The incubation of BSA with U-PS particles resulted in a slight increase in the size of the majority of particles and the generation of a small number of larger particle agglomerates around 500 nm in size. At T180 U-PS particles had begun to self agglomerate, a process which was inhibited in the presence of BSA. This was evident by examining both the z
average and the size distribution by number. RPMI promoted the agglomeration of both particles (see Table 1).

A-PS particles had a positive ZP in TBS with calcium, which reduced slightly over time at 37 °C. The addition of RPMI to the A-PS particles resulted in a negative ZP (Table 1). The addition of SP-A or BSA to the A-PS particles also resulted in negative ZPs (Table 1). The U-PS particle ZP became closer to zero over time and following the addition of RPMI (Table 1). The addition of RPMI promoted the agglomeration of both particles (see Table 1).

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### Table 1. Hydrodynamic size and zeta potential of A-PS and U-PS particles following incubation with SP-A or BSA.

<table>
<thead>
<tr>
<th>Media (time point, min)</th>
<th>Control</th>
<th>SP-A</th>
<th>BSA</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>Z-AVE (d, nm)</td>
<td>Δd (%)a</td>
<td>PDI</td>
</tr>
<tr>
<td>A-PS TBS (T-2)</td>
<td>109.7 –</td>
<td>0.123 +24.4</td>
<td></td>
</tr>
<tr>
<td>TBS (T0)</td>
<td>258.8 135.9</td>
<td>0.426 +14.9</td>
<td></td>
</tr>
<tr>
<td>TBS (T48)</td>
<td>1264 1052.2</td>
<td>0.283 +15.7</td>
<td></td>
</tr>
<tr>
<td>TBS + RPMI (T60)</td>
<td>1693 1443.3</td>
<td>0.340 –12.4</td>
<td></td>
</tr>
<tr>
<td>TBS + RPMI (T180)</td>
<td>2229 1931.9</td>
<td>0.363 –9.3</td>
<td></td>
</tr>
<tr>
<td>U-PS TBS (T-2)</td>
<td>127.6 –</td>
<td>0.008 –26.8</td>
<td></td>
</tr>
<tr>
<td>TBS (T0)</td>
<td>136.5 7.0</td>
<td>0.040 –26.1</td>
<td></td>
</tr>
<tr>
<td>TBS (T48)</td>
<td>151.1 18.4</td>
<td>0.100 –17.0</td>
<td></td>
</tr>
<tr>
<td>TBS + RPMI (T60)</td>
<td>324.2 154.1</td>
<td>0.262 –11.3</td>
<td></td>
</tr>
<tr>
<td>TBS + RPMI (T180)</td>
<td>1037.0 712.7</td>
<td>0.540 –7.5</td>
<td></td>
</tr>
</tbody>
</table>

Z average (Z-AVE), polydispersity index (PDI) and zeta potential (ZP) of polystyrene particles incubated at 37 °C at various time points (T-2 to T180). T-2 represents time point immediately prior to mixing with protein which occurred at T0. Particles – protein suspensions were then incubated for 48 min at 37 °C (T48) before the addition of serum-free RPMI cell culture medium (T60). The particles were then incubated for a further two hours (T180).

\[ \Delta d = (d(t) - d(t-2))/d(t-2). \]

The zeta potential of SP-A in TBS was –10.9 mV at T-2.

**Figure 1.** Dynamic light scattering analysis of the size distributions of 100 nm A-PS and U-PS particles in TBS/RPMI. Size distributions of 100 nm A-PS (A and B) and 100 nm U-PS (C and D) nanoparticles in TBS-RPMI; 12.5 cm2/mL of particles in TBS with 5 mM Ca2+ were mixed with 50 μg/mL BSA (■) or 50 μg/mL SP-A (▲) or TBS only (●) for one hour before being mixed with RPMI (TBS:RPMI: 2:3) and their size distributions immediately measured at 37 °C (A and C, T60) and again two hours later (B and D, T180). The final protein concentration was 10 μg/mL, and nanoparticle concentrations were 2.5 cm2/mL. Size distributions of nanoparticles in TBS only at T-2 are shown as dashed line.
of SP-A or BSA had similar effects in making the U-PS ZPs closer to zero (Table 1).

Due to the large polydispersity indices for the DLS measurements and the differing results when comparing particle agglomeration kinetics, fluorescence microscopy was also used to examine NP agglomeration in buffered saline with or without calcium following incubation with SP-A or BSA. The micrographs show that the U-PS particles remained stable either in the presence or absence of calcium at physiological temperatures (Figure 2). The incubation of U-PS particles with SP-A in the absence of calcium resulted in a small degree of particle agglomeration; however, this agglomeration was greatly enhanced in the presence of 2 mM calcium and SP-A (Figure 2). In order to ascertain whether the effect was specific to SP-A, we performed the experiment with a similar concentration of BSA and observed no agglomeration with or without the presence of calcium (Figure 2). A-PS particles self-agglomerated at physiological temperatures (i.e. 37 °C). This self-agglomeration was inhibited in the presence of SP-A in a calcium-independent manner. However, large agglomerates were still evident when A-PS particles were incubated with BSA (Figure 2).

The association of SP-A with A-PS and U-PS particles was also examined using SDS-PAGE analysis. Particles were incubated with SP-A for 24 hours at 37 °C in TBS containing calcium or EDTA. The particles were then centrifuged and washed twice in the appropriate buffer (i.e. TBS containing Ca or EDTA), and the pellet was examined using reduced SDS-PAGE. This allowed the determination of the hard (i.e. strongly bound) SP-A corona. SP-A strongly associated to U-PS particles and the association independent of calcium. SP-A was found not to strongly associate with the A-PS particles whether in the presence of calcium or EDTA (see Figure S4).

Toxicity of U-PS and A-PS NPs

In order to establish whether particle toxicity could influence cellular uptake of the particles, the effect of the NPs on cellular toxicity was investigated using the tetrazolium dye (MTT) colorimetric assay for cellular growth and viability. RAW264.7 cells were incubated with A-PS and U-PS particles in a range from 1 to 15 cm²/mL and were found not to be toxic to RAW264.7 cells at one hour (A-PS: \( p = 0.85 \) and U-PS: \( p = 0.82 \), Figure S5). Following 24 hours of incubation, the A-PS particles reduced cellular viability (\( p < 0.05 \) for concentrations \( \geq 3.75 \text{ cm}^2/\text{mL} \)), whereas no effect was observed for the U-PS particles (\( p = 0.79 \), Figure S5). The results of the dose response at 24 hours were verified with a clonogenic assay, which showed significant toxicity of the A-PS particles from a concentration of \( \geq 0.23 \text{ cm}^2/\text{mL} (p < 0.05, \text{Figure S6}) \) but not for the U-PS particles when compared with no NP particles present (\( p = 0.34, \text{Figure S6} \)).

A-PS particle association to macrophage-like RAW cells analysed by coherent anti-Stokes Raman spectroscopy

Imaging with coherent anti-Stokes Raman spectroscopy (CARS) was used to quantify the association of unlabelled A-PS particles to the murine macrophage-like RAW 264.7 cells. Some of the NPs were pre-incubated with SP-A (10 \( \mu \)g/mL) for an hour before incubating with the cells. Initial experiments showed that individual 100 nm NPs could not be resolved with enough specificity using this technique (data not shown). However, 200 nm A-PS particles were resolvable and therefore used in this study. The CARS analysis showed that SP-A inhibited the association of the A-PS NPs to the cells (Figure 3A). Quantification of the 200 nm A-PS particles compared with the area of the cells showed that SP-A significantly decreased the association of the A-PS NPs with the cells (\( p = 0.029 \), Figure 3B).

NP uptake into RAW cells and mouse AMs analysed by FACS

To examine the effect of SP-A interaction with 100 nm NPs specifically on cellular uptake, rather than just cellular association, we performed dose-response experiments using a two-fold serial dilution of SP-A from 20 to 0 \( \mu \)g/mL with 100 nm fluorescent U-PS or A-PS NPs using the macrophage-like cell line RAW264.7 in the presence of calcium (Figure 4). Following NP treatment and directly before FACS analysis, the cells were treated with trypan blue, which quenches the fluorescent signal outside the cells (Hartshorn et al., 1994). SP-A significantly increased the uptake of U-PS into the RAW cells at concentrations of \( \geq 10 \mu \text{g/mL} (p < 0.01 \text{ with SP-A } \geq 10 \mu \text{g/mL}) \), whereas the uptake of A-PS was significantly reduced in the presence of SP-A at concentrations of \( \geq 0.156 \mu \text{g/mL} (p < 0.05 \text{ at SP-A } \geq 0.156 \mu \text{g/mL}) \) compared with the absence of SP-A (Figure 4). BSA was used as a non-specific protein control at a concentration of 20 \( \mu \)g/mL for both types of particles. BSA caused non-significant increases in the uptake of both U-PS particles (3.8% increase, \( p = 0.44 \)) and A-PS particles (9.1% increase, \( p = 0.19 \); data not shown).

The effect of SP-A on the uptake of A-PS and U-PS in the AMs from wild type (WT) and SP-A knock-out mice (SP-A\(^{-/-}\)) was also examined. An increase in the uptake of 100 nm A-PS particles in AM from SP-A\(^{-/-}\) mice was observed when
Figure 3. The association of 200 nm unlabelled A-PS with (w) and without (w/o) SP-A to macrophage-like RAW264.7 cells visualised and quantified by CARS. (A) CARS images; 200 nm A-PS particles show up as white particles (arrows). Note that other -CH$_2$-rich structures, such as the nuclear membrane, shows up as a visible ring in each cell (asterisks). (B) CARS images were analysed using MATLAB software as described in the materials and methods section. N = 4 per column. Shown is the mean ± standard derivation, $p < 0.05$ was considered statistically significant.

Figure 4. The effect of exogenous SP-A on the uptake of 100 nm A-PS and U-PS particles in macrophage-like RAW264.7 cells. Two-fold serial dilution of SP-A was incubated with fluorescent 100 nm A-PS or U-PS particles (3.8 cm$^3$/mL) in the presence of calcium before incubating with RAW cells. Extra cellular association of NPs with cells were quenched using trypan blue. The particle uptake was analysed using FACS. Shown are the mean ± standard derivation of four independent experiments. *$p < 0.05$ and ****$p < 0.0001$.

Discussion

We have previously characterised the interaction between SP-D and PS particles with different surface modifications (Kendall et al., 2013). This showed that SP-D differentially interacts with particles, modifying their uptake by AMs and lung-derived dendritic cells. The purpose of this study was to investigate whether SP-A showed differential interaction with PS NPs with different surface charge and if this interaction affected uptake of these NPs into macrophages in a similar or complementary way to SP-D.

NP characterisation

The size of SP-A in water remained stable at around 30 nm, which is consistent with the literature, where human SP-A has previously been measured by DLS to be 42 ± 6 nm (López-Sánchez et al., 2011) and electron micrographs of recombinant human SP-A being less than 50 nm in length (Voss et al., 1988).

The incubation of U-PS particles with SP-A or BSA resulted in the ZPs of the particle suspensions moving closer to zero. This shows that the addition of protein to the particle suspension results in a reduction in colloidal stability, a process which enhances the likelihood of particle agglomeration. This observation is similar to the findings by Ruge et al (2011), where they observed that SP-A and BSA had similar effects when incubated with magnetite NPs with different surface charges. In this study, SP-A changed the ZP for A-PS particles from a positive to a negative charge when incubated in TBS with calcium (+24.4 to −7.4 mV) or nanopure water (+60 to −22.8 mV). This is also similar to the findings by Ruge et al. (2011) when using particles with a positive ZP.

Protein coronas, which form around NPs, usually consist of an outer layer of loosely associated proteins termed the ‘soft’ corona and an inner layer of strongly associated proteins called the ‘hard’ corona (Barran-Berdon et al., 2013; Deng et al., 2012). Differences in particle agglomeration following incubation with SP-A may be linked to altered protein association with the particles. In particle association studies using SDS PAGE, we found that SP-A formed a hard corona around U-PS but not A-PS particles (Figure S4). The changes in the DLS and ZP measurements suggest that SP-A forms a soft corona around the A-PS particles. This shows that differences in the particle surface chemistry can influence the interaction of SP-A with the particles, which in turn may influence particle agglomeration and uptake. Furthermore, this study has shown that although SP-A-mediated agglomeration of U-PS particles depends on the presence of calcium, the association of SP-A with these particles is calcium independent. Although the ZP for both NPs bound by SP-A is around −20 mV in nanopure water and around −10 mV in TBS, the agglomeration kinetics are different. The U-PS particles agglomerated in the presence of SP-A, whereas disagglomeration
experiments with and B) and two (Figure 5C) independent derivation derived from three (Figure 5A)
mean fluorescence intensity (MFI) ± standard statistical significant and significant values
are shown in the figure. Data show relative AMs from wild-type mice and SP-A grey) or presence (dark grey) of SP-A with
surface of the CRD of the SP-A becomes less negatively charged
modelling, Head et al. (2003) showed that the electrostatic structure of trimeric fragment of rat SP-A and computer
U-PS particles. Calcium is required to stabilise the conformation of the lectin-binding domain (Head et al., 2003). By using the
In the case of A-PS particles, the results indicate that the presence of the SP-A molecule at the particle surface may block the sites on the particle involved in self-agglomeration. SP-A would thereby inhibit A-PS self-agglomeration. The degree to which this is an SP-A-specific effect is unclear as BSA also inhibits A-PS agglomeration. Further work examining the particle agglomeration kinetics following SP-A incubation is necessary using techniques that allow the accurate quantification of particle size in highly polydisperse suspensions.

**SP-A-mediated agglomeration of U-PS is dependent on calcium concentration**

We found that a minimum concentration of 2 mM calcium was required for SP-A to agglomerate the 100 nm U-PS particles (Figure S3). This minimum calcium concentration is consistent with findings reported by Haagsman et al. (1990) who observed that SP-A became saturated with calcium around a free calcium concentration of 2 mM. This also agrees with structural findings reported for the recombinant fragment of human SP-D, where this calcium concentration was thought to act like a molecular switch in the lectin-binding site (Shrive et al., 2003). These findings indicate that the CRD may be involved in the agglomeration of the U-PS particles. Calcium is required to stabilise the conformation of the lectin-binding domain (Head et al., 2003). By using the structure of trimeric fragment of rat SP-A and computer modelling, Head et al. (2003) showed that the electrostatic surface of the CRD of the SP-A becomes less negatively charged when calcium is present in the CRD. The SP-A-induced agglomeration of NPs might not directly involve the actual lectin binding site in the CRD region, but the overall conformation or electrostatic surface charge induced by calcium could result in a differential interaction than that seen in the absence of calcium. We have previously shown that a recombinant fragment of SP-D, containing a trimeric unit of neck and CRD regions only (Figure S1), is enough to interact with the particles used in this study (Kendall et al., 2013). It therefore seems plausible to extend this finding to SP-A. SP-A would, by crosslinking individual particles via individual trimeric units, be able to agglomerate NPs. These results also show that SP-A has a different interaction with surface-modified NPs compared with native SP-D. SP-A inhibits the agglomeration of A-PS particles, whereas SP-D facilitates A-PS particle agglomeration. Both SP-A and SP-D agglomerated U-PS particles in the presence of calcium (summarised in Figure 6A).

**NP toxicity**

We show here that the used A-PS and U-PS particles were not toxic to the RAW 264.7 cells over short incubation periods such as those used in the *in vitro* cellular experiments (Figure S5 and S6). The observed difference between in the effect of SP-A on A-PS and U-PS particles is therefore not due to the toxicity of short-term exposure of the cells with the NPs. However, when extending the incubation period from 1 hour to 24 hours, the A-PS particles did show toxic effects on the cells, while no toxic effect was observed for the U-PS particles. This is consistent with previous reports where it was observed that A-PS, but not U-PS, particles had a toxic effect on the TTI cell line, a human alveolar epithelial type I like cell line (Ruenraroengsak et al., 2012). This highlights the difference between the ‘high dose–short exposure’ acute toxicity models often used in *in vitro* assays and real-life exposure scenarios where there is often low concentration of NPs but a long/chronic exposure period.
It has been shown that both lipids and proteins from surfactant interact with NPs (Bakshi et al., 2008; Kendall, 2007). In order to create a more realistic in vitro model of in vivo conditions, it would be beneficial to include lipids in these models for future experiments. Ruge et al. (2012) looked at SP-A and SP-D with metal-NPs with different surface coatings and found differential effects of SP-A and SP-D. They also observed that incorporating surfactant lipids into the in vitro models modified the effects of SP-A and SP-D (Ruge et al., 2012). This highlights the fact that current in vitro models do not reflect what happens in vivo. Human BAL can agglomerate NPs (Kendall et al., 2002). An in vitro model using the natural porcine surfactant preparation Curosurf (devoid of SP-A and SP-D) also modified the effect of multi-walled carbon nanotubes and enhanced their oxidative and pro-inflammatory effects (Gasser et al., 2012). In order to have a comprehensive understanding of how NPs interact with both surfactant proteins and lipids, it is important to understand how NPs interact not only with specific subcomponents of surfactant but also implementing a model system that resembles in vivo circumstances as recently highlighted by Schleh et al. (2013). Agglomeration seems to be the key to enhanced uptake into AMs in these observations and the surface chemistry described provides a mechanism for agglomeration by SP-A. However, SP-A provides important immune functions within the airspace and sequestering by NPs may leave an individual vulnerable to other pathogenic events and uncontrolled inflammation. We have
previously shown that three different types of carbon black particles, ranging from 25 to 75 nm in diameter, were able to completely eliminate SP-D from a suspension (Kendall et al., 2004). Furthermore, an animal study exposing rats infected with *Streptococcus pneumoniae* to PM$_{2.5}$ particles resulted in an exacerbation of the on-going infection (Zelikoff et al., 2003). We have recently shown that incubating these NPs with SP-A and SP-D alters the ability of these proteins to neutralise influenza A infection *in vitro* (McKenzie et al., 2015). This implies that sequestering immune-related proteins could result in functionally deficient individuals resulting in an increase in their susceptibility towards bacterial and viral infections and other inflammatory conditions as observed in mice deficient for SP-A or SP-D (Hawgood et al., 2004; LeVine & Whitsett, 2001; Li et al., 2002).

It is therefore important that more research is performed to elucidate the implications of the interactions between SP-A and -D and NPs in order to evaluate the potential health implications when implementing the usage of NPs in the working environment and everyday modern consumer products.

**Conclusions**

In this study, we have characterised the interaction between NPs and SP-A, examined the effect on cellular uptake, and propose uptake mechanisms into macrophages. SP-A showed material-specific binding and calcium-dependent agglomeration of U-PS NPs. We showed that SP-A inhibited the uptake of 100 nm A-PS NPs into macrophage-like cells and primary AMs using CARS (unlabelled 200 nm NPs) and FACS (fluorescent NPs), but this was not observed for larger (500 nm) A-PS particles.

This study combined with previous studies with SP-A and SP-D shows that these molecules may have a (complementary) role in clearing non-pathogen particulate and nanoparticulate materials *in vivo*. An important factor, when examining the interaction of SP-A or SP-D with NPs, is to consider how the interplay between surfactant lipids and proteins in the bio-corona will affect the interaction and the subsequent downstream bioavailability of the collectins. Future *in vivo* studies focusing on the interaction between these lung collections, NPs and the clearance route(s) into cells and body compartments is required to provide further insight into the role(s) of SP-A and SP-D in response to inhalation of NPs.

**Acknowledgements**

S. M. acknowledges EPSRC Laser Loan Pool support, which enabled the CARS experiments. M. K., H. W. C. and J. M. developed the concepts in all the detailed experiments. M. K., H. W. C. and J. M. wrote and managed the proposal outlining the experimental design. M. G. and C. M. organised and collected the human BAL. Z. M., H. W., C. E. and P. D. prepared the materials and conducted DLS. Z. M., M. K., H. W., C. E. and P. D. jointly interpreted and synthesised the protein-NP data to form conclusions. Z. M., R-M. M., H. W. C. and J. M. designed the RAW264.7 and alveolar macrophage experiments. Z. M. and R-M. M. conducted the RAW264.7 and alveolar macrophage experiments. S. M. performed the CARS experiments and the analysis Z. M., M. K. and J. M. jointly interpreted and synthesised the cell data to form the protein-NP manuscript. Z. M., M. K., R-M. M., H. W. C. and J. M. jointly interpreted and synthesised the protein-NP manuscript. Z. M., M. K., R-M. M., H. W. C., C. E., P. D., M. G., C. M., S. M., H. W. C. and J. M. jointly revised the manuscript critically for important intellectual content. We thank Dr. Tony Willis for the N-terminal sequencing of purified native human SP-A.

**Declaration of interest**

The authors do not have any competing financial interests with the work in this article.

This work was funded under the Joint Environment and Human Health programme (NERC-EPSC Research Project NE/003935-1), funded by agencies of the UK Government: The Natural Environment Research Council (NERC), Department for Environment Food and Rural Affairs (Defra), Environment Agency (EA), Ministry of Defence (MOD) and the Medical Research Council (MRC). We gratefully acknowledge the financial support of the MRC ITTP Toxicology Unit for Z. M. The use of FENAC (Facility for Environmental Nanoscience Analysis and Characterisation) was supported by NERC FENAC access grant 2013/05/004. This work was also supported by the National Institute of Health Research (NIHR) funded Respiratory Biomedical Research Units of University Hospital Southampton and the Royal Brompton and Harefield NHS Foundation Trust.

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Supplementary material available online
Supplementary Table S1 and Figures S1–S6.

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