UNIVERSITY BIRMINGHAM University of Birmingham Research at Birmingham

PRaVDA

PRaVDA Consortium

DOI: 10.1016/j.nima.2015.12.013

License: Creative Commons: Attribution-NonCommercial-NoDerivs (CC BY-NC-ND)

Document Version Peer reviewed version

Citation for published version (Harvard):

PRaVDA Consortium 2016, 'PRaVDA: high energy physics towards proton computed tomography', *Nuclear Instruments & Methods in Physics Research. Section A. Accelerators, Spectrometers, Detectors.* https://doi.org/10.1016/j.nima.2015.12.013

Link to publication on Research at Birmingham portal

Publisher Rights Statement: Eligibility for repository: checked 10/02/16

General rights

Unless a licence is specified above, all rights (including copyright and moral rights) in this document are retained by the authors and/or the copyright holders. The express permission of the copyright holder must be obtained for any use of this material other than for purposes permitted by law.

•Users may freely distribute the URL that is used to identify this publication.

Users may download and/or print one copy of the publication from the University of Birmingham research portal for the purpose of private study or non-commercial research.
User may use extracts from the document in line with the concept of 'fair dealing' under the Copyright, Designs and Patents Act 1988 (?)

•Users may not further distribute the material nor use it for the purposes of commercial gain.

Where a licence is displayed above, please note the terms and conditions of the licence govern your use of this document.

When citing, please reference the published version.

Take down policy

While the University of Birmingham exercises care and attention in making items available there are rare occasions when an item has been uploaded in error or has been deemed to be commercially or otherwise sensitive.

If you believe that this is the case for this document, please contact UBIRA@lists.bham.ac.uk providing details and we will remove access to the work immediately and investigate.

Author's Accepted Manuscript

PRaVDA: High Energy Physics towards proton Computed Tomography

T. Price



PII:S0168-9002(15)01584-3DOI:http://dx.doi.org/10.1016/j.nima.2015.12.013Reference:NIMA58412

To appear in: Nuclear Inst. and Methods in Physics Research, A

Received date: 24 June 2015 Revised date: 2 December 2015 Accepted date: 10 December 2015

Cite this article as: T. Price, PRaVDA: High Energy Physics towards protot Computed Tomography, *Nuclear Inst. and Methods in Physics Research, A* http://dx.doi.org/10.1016/j.nima.2015.12.013

This is a PDF file of an unedited manuscript that has been accepted fo publication. As a service to our customers we are providing this early version o the manuscript. The manuscript will undergo copyediting, typesetting, and review of the resulting galley proof before it is published in its final citable form. Please note that during the production process errors may be discovered which could affect the content, and all legal disclaimers that apply to the journal pertain

PRaVDA: High Energy Physics towards proton Computed Tomography

T. Price^{a,b,*}

^aSchool of Physics and Astronomy, University of Birmingham, Birmingham, B15 2TT, UK ^bOn behalf of the PRaVDA Consortium

Abstract

Proton radiotherapy is an increasingly popular modality for treating cancers of the head and neck, and in paediatrics. To maximise the potential of proton radiotherapy it is essential to know the distribution, and more importantly the proton stopping powers, of the body tissues between the proton beam and the tumour. A stopping power map could be measured directly, and uncertainties in the treatment vastly reduce, if the patient was imaged with protons instead of conventional x-rays. Here we outline the application of technologies developed for High Energy Physics to provide clinical-quality proton Computed Tomography, in so reducing range uncertainties and enhancing the treatment of cancer.

Keywords: Tracking detectors, Proton radiotherapy, CMOS, High Energy Physics, Proton Computed Tomography, Applications *PACS:* 11.30.Rd, 87.55.Gh, 87.57.Q-, 87.55.-x

31

32

58

59

60

1. Introduction

Proton radiotherapy uses beams of protons, typically with en- 33 ergies between 70 and 230 MeV, to treat cancer. Compared to 34 conventional x-ray radiotherapy, proton radiotherapy can deliver a larger dose to the tumour region with a reduced dose to 5 the healthy surrounding tissue due to the Bragg Peak (BP). To 6 ensure that the protons stop within the target volume it is essential to know the proton stopping powers of the body tissues traversed by the beam on the way to the tumour. Conventionally, 38 9 this information is acquired using an x-ray Computed Tomog-10 raphy (CT) scan. Conversions to proton stopping power from 40 11 Hounsfield Unit can lead to a typical uncertainty on the proton 12 range of 3.5 % [1] and could lead to sub-optimal patient treat-13 ment. Performing a CT scan using protons, a proton CT (pCT), 43 14 would allow the stopping power to be measured directly and the $_{44}$ 15 range uncertainties greatly reduced. 16 The PRaVDA Consortium, funded by the Wellcome Trust, 46 17 are developing a proof of principle pCT instrument. In order 47 18 to reconstruct a pCT the input and output trajectories of every $_{_{48}}$ 19

single proton must be measured alongside the residual energy 49 20 of the proton once it has interacted with the patient. We envis-21 age that 3.5×10^9 reconstructed protons and a delivered dose of ₅₁ 22 2 cGy per image will allow uncertainties on the stopping power 23 of ± 1 %. High speed readout electronics are required in order 53 24 to keep data acquisition times at clinically feasible scales. Full 25 details of the required specifications for pCT are given here [2]. 55 26 PRaVDA aim to fully reconstruct more than 1M protons/s by 27 using technologies developed for High Energy Physics (HEP). 28 This would yield a total scan time of 60 minutes. The remain- 56 29

³⁰ der of these proceedings will outline: the strip sensors used for

Preprint submitted to Elsevier

proton tracking (Section 2); the CMOS sensors used to measure the residual energy (Section 3), and the Geant4 model developed to optimise the PRaVDA instrument (Section 4). Finally the future scope of the project will be discussed (Section 5).

2. Strip Tracking Sensors

The PRaVDA tracking system uses silicon strip detectors developed by the HEP group at the University of Liverpool and fabricated with high yield by Micron Semiconductor Ltd. The tracking system consists of four modules, two before the patient and two afterwards. Within each module, three sensors are rotated at 60° relative to each other to allow the reconstruction of proton tracks in an x-u-v co-ordinate system. This configuration vastly reduces ambiguities at higher beam fluences. The strip detectors are 150 μ m thick n-in-p silicon with a strip pitch of 90.8 μ m. The sensor is split in half, with a strip length of 48 mm to enable a maximum readout rate of 104 MHz. A total active area of 93×96 mm² is achieved using 2048 strips, read out by 16 ASICs (8 for each strip half). A double threshold readout further assists in the untangling of ambiguities caused by multiple protons being collected in the same strip. Further information can be found here [3]

A single layer of strips were tested using the University of Birmingham MC40 cyclotron with 36 MeV protons. The measured 1D profile for a 40mm diameter beam (Figure 1) is in good agreement with the delivered beam.

3. CMOS Range Telescope

Pixelated sensors allow multiple protons to be tracked simultaneously and can offer a reduced image acquisition time compared to scintillators. The CMOS Range Telescope (RT) is a stack of large scale CMOS Active Pixel Sensors (APS).

^{*}Corresponding author Email address: t.price@bham.ac.uk (T. Price)



Figure 1: Channel by channel count of the number of detected proton signals per strip. Inset is a scanned GaFChromic film normalised to maximal dose used to measure the beam profile.

Full CMOS capability is achieved due to the use of deep-well 61 technology as developed for HEP devices such as those pro- 99 62 posed for digital calorimetry at the ILC [4] or the ALICE ITS_{100} 63 upgrade [5]. The proton's position is measured in each layer 10164 whilst a finite amount of its energy is also lost. The final layer₁₀₂ 65 in which a proton is detected before it stops will yield the resid-103 66 ual range (and therefore the energy) of the proton. The $CMOS_{104}$ 67 layers can be interleaved with Perspex sheets to increase the to-105 68 tal range of the RT. PRaVDA have demonstrated the ability of₁₀₆ 69 using CMOS to track protons between layers [6][7], and mea-107 70 sure an increasing proton signal as the proton energy falls [8]. 108 71 The CMOS APS developed by PRaVDA is known as Pria-109 72 *pus.* Priapus has an active area of $50 \times 100 \text{ mm}^2$ with a pixel₁₁₀ 73 pitch of $194 \times 194 \,\mu\text{m}^2$. The wafer is 750 μm thick with a sensi-74 tive epitaxial layer of 18 μ m. Each pixel contains five diodes to₁₁₂ 75 maximise the charge collection efficiency. A full frame readout₁₁₃ 76 rate of 1000 frames/s is possible and the RT will unambigu-77 ously track more than 1000 protons per frame. Pripaus is three 78 side buttable yielding the potential of a single RT layer to have114 79 a total sensitive area of 10×20 cm². 80

The pixel values are represented in arbitrary units of Digital Number (DN). The first beam test with a single second generation Priapus sensor in May 2015 demonstrated a sensor gain of 45 e⁻/DN and a noise floor of 4 DN (180 e⁻). Figure 2 shows the detected signal size for 29 MeV protons when the cluster size is greater than one pixel. A SNR of 25 has been observed.

87 4. Geant4 Model

A Monte Carlo simulation (SuSi) has been developed using₁₂₃ Geant4.10 with readout implemented using ROOT. It contains₁₂₄ 89 realistic beam line models for the two proton sources where125 90 the device will be tested (iThemba LABS, SA and University¹²⁶ 91 of Birmingham, UK), full device geometry, and realistic read₁₂₈ 92 out for both the strip and CMOS sensors. Each component of129 93 the simulation has been verified against data. The simulation¹³⁰ 94 allows our device parameters to be optimised to achieve the best¹³¹ 95 possible pCT with our technology and the testing of our novel 96

Observed Proton Signal Size for 29 MeV Protons



Figure 2: The reconstructed signal size (Cluster Value) for all 29 MeV protons which caused more than one pixel to fire.

5. Outlook

We have demonstrated the ability to detect protons in a single layer of both our new strip sensors and CMOS devices. Following on from this work the strip detector modules are being assembled and tested using both radioactive sources and the University of Birmingham cyclotron to illustrate the ability to fully reconstruct beam profiles in x-u-v space. Multiple strip modules will then form proton tracks which will be projected into the Priapus sensors. By the end of 2015 we aim to have a fully instrumented device which will allow us to acquire a pCT of an animal phantom on a clinical timescale using technology adapted from the HEP community. Finally, (we hope) the knowledge accumulated through this project will lead to a commercialised device which will be routinely used in a clinical environment, reducing the uncertainties on proton radiotherapy treatments and aiding the treatment of cancer.

Acknowledgments

This work was supported by the Wellcome Trust Translation Award Scheme, grant number 098285. The authors wish to thank aSpect Systems GmbH and ISDI Limited for their support and development of the PRaVDA system. The authors would also like the thank the cyclotron operators at the University of Birmingham for providing the beams that made this work possible.

References

- [1] M. Yang, et al., Phys. Med. Biol. 57 (2012) 4095.
- [2] G. Poludniowski, et al., Br. J. Radiol. (2015) [Epub ahead of print]
- [3] J. T. Taylor, et al., JINST 10 (2015), C02015
- [4] T. Price, et al., JINST 8 (2013), P01007
- [5] L. Molnar, JINST 9 (2014), C12023
- [6] G. Poludniowski, et al., Phys. Med. Biol. 59 (2014) 2569
- [7] M. Esposito, et al., JINST 10 (2015) C06001
- [8] T. Price, et al., JINST 10 (2015), P05013
- [9] G. Poludniowski, et al., Phys. Med. Biol. 59 (2014) 7905.

122