

Between-day reliability of trunk orientation measured with smartphone sensors during sit-to-stand in asymptomatic individuals

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DOI:

[10.1016/j.msksp.2022.102713](https://doi.org/10.1016/j.msksp.2022.102713)

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Document Version

Peer reviewed version

Citation for published version (Harvard):

Gordon, S, Kind, O, Singh, G, Wood, A & Gallina, A 2022, 'Between-day reliability of trunk orientation measured with smartphone sensors during sit-to-stand in asymptomatic individuals', *Musculoskeletal Science and Practice*. <https://doi.org/10.1016/j.msksp.2022.102713>

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1 **Title: Between-day reliability of trunk orientation measured with smartphone sensors during sit-to-**
2 **stand in asymptomatic individuals**

3

4 **ABSTRACT:**

5 **Background.** Trunk kinematics during sit-to-stand is often impaired in individuals with musculoskeletal
6 disorders. Trunk kinematics is commonly assessed in laboratories using motion capture; however, this
7 equipment is often not available outside research centers. Smartphones are widely available and may be
8 a suitable alternative to assess trunk orientation during sit-to-stand remotely.

9 **Objectives.** We investigated whether trunk orientation in the sagittal plane during sit-to-stand can be
10 measured reliably between days when collected remotely using smartphones.

11 **Design.** Cross-sectional study.

12 **Method.** Forty-three asymptomatic participants performed 15 sit-to-stand movements in two separate
13 sessions remotely over videoconferencing. Trunk orientation was measured using each participant's
14 smartphone. Absolute peak trunk orientation in the sagittal plane was extracted during standing, sitting,
15 stand up and sit down. Relative trunk orientation was calculated as the difference between sitting and
16 stand up, or sitting and sit down. Reliability was assessed using Intraclass Correlation Coefficient ($ICC_{2,k}$),
17 Standard Error of Measurement (SEM) and Minimal Detectable change (MDC). Between day bias and
18 between-gender differences were assessed using T tests.

19 **Results.** All measures showed good reliability ($ICC_{2,k}>0.80$; $SEM<5.6$ degrees; $MDC<13.6$ degrees) and no
20 between-day bias ($p>0.31$). Relative measures were more consistent ($ICC_{2,k}>0.88$; $SEM<3.6$ degrees;
21 $MDC<9.9$ degrees). No between-gender differences were observed for relative orientation ($p>0.75$).

22 **Conclusions.** Sagittal trunk orientation during sitting, standing, and sit-to-stand can be measured reliably
23 when asymptomatic individuals use their own smartphones supervised over videoconferencing. These
24 findings support the use of smartphone sensors for assessing how trunk orientation changes over time,
25 which may assist physiotherapists assess movement patterns of individuals with musculoskeletal
26 disorders remotely.

27

28 **Keywords:** Smartphone, trunk, kinematics, sit-to-stand, reliability.

29 **INTRODUCTION:**

30 Sit-to-stand is a daily living activity commonly impaired in individuals with musculoskeletal symptoms
31 (Baldwin et al., 2017; Yenişehir et al., 2020). Forward transition of the center of mass is obtained by
32 flexion of the trunk, which has been shown to be impaired in individuals with low back pain (Sedrez et
33 al., 2019), knee osteoarthritis (Sonoo et al., 2019), and in the elderly (Dubost et al., 2005; Jeon et al.,
34 2021). Strategies with excessive or insufficient trunk flexion have been described in the elderly (van der
35 Kruk et al., 2021), and the inability to move the center of mass forward has been linked to unsuccessful
36 sit-to-stand performance (Kerr et al., 2019). Objective measures of trunk orientation during sit-to-stand
37 may assist clinicians in assessing motor impairments and to monitor the effectiveness of physiotherapy
38 interventions.

39 Trunk kinematics, which includes trunk orientation (e.g.: angle between the trunk and the vertical) and
40 thoraco-lumbar flexion (i.e.: angle between the thoracic and the lumbar spine), is usually assessed using
41 motion capture (Christe et al., 2022; Kerr et al., 2019; Sedrez et al., 2019) and inertial measurement
42 sensors (Roldán-Jiménez et al., 2019). These technologies are often not available outside research
43 laboratories. Smartphone sensors, instead, are widely available to the general population and have been
44 shown to provide valid (Elgueta-Cancino et al., 2022; Keogh et al., 2019; Sedrez et al., 2020) and reliable
45 (Elgueta-Cancino et al., 2022; Keogh et al., 2019; Sedrez et al., 2020) measures of body segment
46 orientation, especially in static tasks. While several acceleration parameters were shown to be reliable
47 when measured with a smartphone during a dynamic task such as sit-to-stand (Cerrito et al., 2015), it is
48 currently unknown if trunk orientation measures obtained with smartphone sensors are also reliable. In
49 addition, the vast majority of studies using smartphone sensors to measure kinematics has been
50 performed in a laboratory, where the same smartphone was placed on the participant by an
51 experienced researcher (Elgueta-Cancino et al., 2022; Keogh et al., 2019; Sedrez et al., 2020). It is

52 currently unknown whether reliable trunk orientation measures can be obtained in a more ecological
53 setting, when individuals measure their kinematics using their own smartphone remotely.

54 In this study we investigated whether trunk orientation in the sagittal plane during sitting, standing, and
55 sit-to-stand can be measured remotely using smartphone sensors, and whether the measures are
56 reliable between days.

57

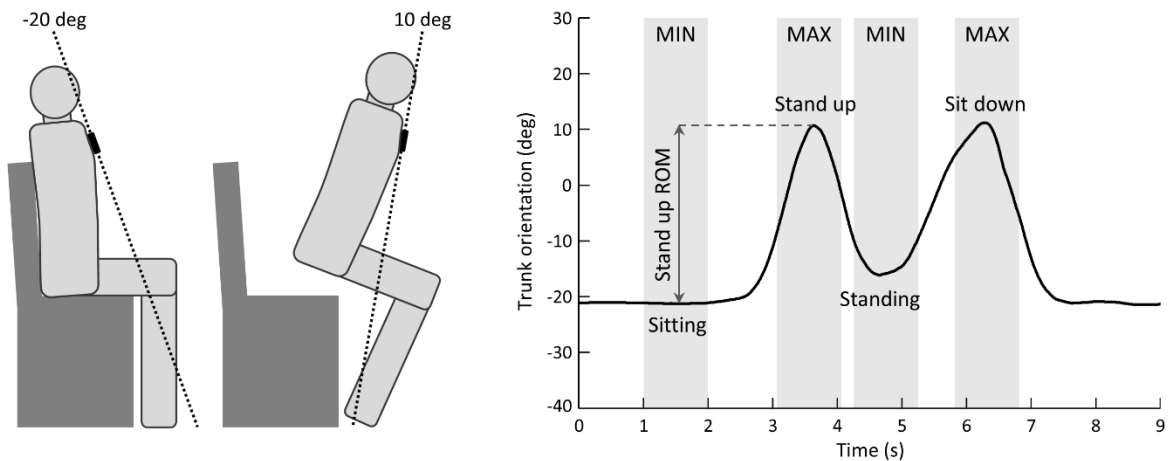
58 **METHODS:**

59 Forty-three adults (29 women; age: 26.7 ± 12.3 ; height: 171.3 ± 8.4 cm; weight: 72.4 ± 17.9 kg) who reported
60 no current pain, injury, or known motor impairment participated in two sessions at least a week apart.
61 Participants were recruited from the student population of the XXX and from the community, and
62 individuals who reported previous injury or pain but were currently asymptomatic were allowed to
63 participate. This study was approved by the ethics committee of the XXX, and participants signed an
64 informed consent before participating in the study.

65 Participants performed 3 sets of 5 sit-to-stand movements at a self-selected pace, wearing the same shoes
66 and using the same chair in the two sessions, under supervision of a researcher via videoconferencing.
67 The participants were free to choose where to perform the experimental session, for instance in their
68 residence or elsewhere, and there were no restrictions with respect to the height of the chair. The number
69 of repetitions was conservatively chosen as the largest number of trials reported in a recent systematic
70 review (Pourahmadi et al., 2019). Each participant collected trunk orientation data using the Matlab
71 Mobile app (MathWorks, Natick, US) installed in their own smartphone. We asked the participants to hold
72 their smartphone on their upper chest using both hands during the task. Participants were instructed to
73 stand up and sit down at their own pace, and to ensure that their back would touch the chair backseat
74 every time they sat down. The smartphone position was standardized (landscape orientation, screen

75 facing forward, camera on the left) so that changes in trunk orientation in the sagittal plane would be
76 recorded as changes in Roll angle (Orientation sensor). Since 0 degrees corresponded to a vertical
77 orientation of the smartphone, value of -20 degrees would indicate that the front of the participant chest
78 was tilted 20 degrees from the vertical towards extension (Figure 1). The data was digitized 100 Hz and
79 shared with the researchers through Matlab Drive (MathWorks, Natick, US).

80 The data was exported in csv format using a custom-made script in Matlab Online (MathWorks, Natick,
81 US) to be analyzed in Microsoft Excel (Microsoft corporation, Redmond, US). For each repetition, we
82 visually identified the following phases of the sit-to-stand movement: i) Sitting, before the start of the
83 movement; ii) Stand up, first peak of trunk flexion; iii) Standing, trough between the two flexion peaks; iv)
84 Sit down, second peak of trunk flexion. Maximum and Minimum functions were used to extract the exact
85 value in each visually-identified phase. These absolute orientation values were averaged across 15
86 repetitions, separately for day 1 and day 2. As an estimate of relative orientation, Stand up range of
87 motion (ROM) and Sit down ROM were calculated as the difference between Sitting and Stand up, or
88 Sitting and Sit down, respectively. Since the changes in angle between sternum and thoracic spine are
89 expected to be minimal during sit-to-stand, sensors placed on the sternum or on the thoracic spine will
90 provide similar relative orientation estimates (although absolute measures will have a subject-specific bias
91 equal to the angle between sternum and thoracic spine).



92

93 *Figure 1: Left: Protocol and smartphone position. Right: Example of trunk orientation of one participant.*
 94 *Shaded areas depict where the maximum (Stand up, Sit down) and minimum (Sitting, Standing) values*
 95 *were identified to quantify kinematics during sit-to-stand.*

96

97 Using SPSS (IBM, Armonk, version 28), we assessed the between-day reliability as: i) two-way random
 98 effect Intraclass Correlation Coefficient for absolute agreement and average measures ($ICC_{2,k}$); ii) standard
 99 error of measurement (SEM); iii) minimal detectable change (MDC) (de Vet et al., 2011). We estimated
 100 the between-day bias using paired T-tests. To understand whether gender influenced our estimates, we
 101 compared the absolute and relative trunk orientation between males and females using independent T-
 102 tests on the data from day 1. Significance was set at $\alpha = 0.05$, and all data is reported as mean and
 103 standard deviation.

104

105 **RESULTS:**

106 Thirty-four participants used an Apple iPhone and 9 participants used an Android-based smartphone. Data
 107 was normally distributed (Shapiro-Wilk test). Values, reliability statistics and comparison by gender results
 108 are summarized in table 1, and Bland-Altman plots are shown in Figure 2.

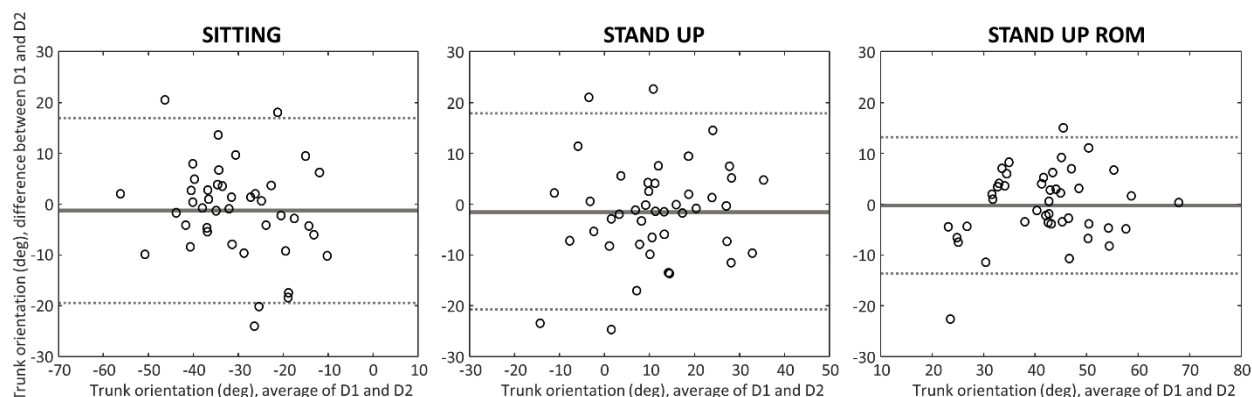
109 While all measures showed good reliability ($ICC_{2,k} > 0.80$), relative orientation measures showed larger ICC
 110 with narrower confidence intervals, lower SEM and MDC. No between-day bias was observed (Stand up:
 111 $p=0.31$; Sit down: $p=0.42$; Standing: $p=0.52$; Sitting: $p=0.36$; Stand up ROM: $p=0.82$; Sit down ROM:
 112 $p=0.84$). When comparing orientation estimates between genders, trunk flexion was approximately 10
 113 degrees larger in males in the absolute (Stand up: $p=0.012$; Sit down: $p=0.017$; Standing: $p=0.004$; Sitting:
 114 $p=0.001$), but not in relative (Stand up ROM: $p=0.756$; Sit down ROM: $p=0.751$) orientation measures.

115 *Table 1: Between day reliability, bias, and gender difference in sagittal trunk orientation and range of*
 116 *motion during sit-to-stand. * $p < 0.05$*

Phase	Value (deg)	ICC [CI]	SEM (deg)	MDC (deg)	Between-day bias (deg)	Between-gender difference (deg)
Absolute reliability measures						
Standing	-24.1±10.6	0.80 [0.64-0.89]	4.7	13.1	-1.0±9.6	9.8 *
Sitting	-31.0±10.7	0.82 [0.66-0.90]	4.6	12.7	1.3±9.2	10.9 *
Stand up	10.7±13.4	0.83 [0.68-0.91]	5.6	15.4	1.5±9.8	9.7 *
Sit down	10.8±13.0	0.86 [0.74-0.92]	4.9	13.6	1.1±8.9	9.9 *
Relative reliability measures						
Stand up ROM	41.7±11.4	0.89 [0.79-0.93]	3.6	9.9	0.2±6.9	-1.2
Sit down ROM	41.8±9.7	0.88 [0.77-0.93]	3.3	9.1	-0.2±6.3	-1.0

117

118



119 *Figure 2: Between-day reliability for sitting, stand up, and stand up range of motion. In the Bland-Altman*
 120 *plots, each circle represents the average of (X axis) and difference between (Y axis) estimates of trunk*
 121 *orientation for each participant. The thick gray line represents the average difference between days, and*
 122 *the dashed lines depict the 95% limits of agreement. D1 and D2 identify day 1 and day 2.*
 123

124

125 **DISCUSSION:**

126 Our findings show good between-reliability of trunk orientation measured remotely using smartphone
127 sensors during sit-to-stand, especially when relative measures of range of motion is considered. The
128 good between-day reliability is consistent with other smartphone-derived measures obtained in the
129 laboratory (Cerrito et al., 2015; Elgueta-Cancino et al., 2022; Keogh et al., 2019; Sedrez et al., 2020), with
130 measures of lumbar motion obtained using motion capture in individuals with and without low back
131 pain (Pourahmadi et al., 2018), and with trunk motion measured by different raters using commercially
132 available inertial measurement units (Hamersma et al., 2020). Although the current protocol did not
133 allow to test whether the measure is valid, the relative trunk orientation values close to 40 degrees
134 observed here are similar to those measured in the laboratory using IMUs (Roldán-Jiménez et al., 2019)
135 and motion capture (Dubost et al., 2005). The inter-individual variability in relative trunk orientation of
136 10-11 degrees is similar to the 12-13 degrees reported when using IMUs in the laboratory (Roldán-
137 Jiménez et al., 2019), whereas the lower variability of approximately 5 degrees reported by others
138 (Dubost et al., 2005) may be due to differences in the protocol.

139 While all measures demonstrated good reliability, absolute measures were consistently biased toward
140 posterior tilt (trunk extension) in females. This gender difference may be explained by anatomical
141 factors, such as chest anatomy. In females, breast may have increased the distance between the bottom
142 of the smartphone and the sternum, resulting in increased posterior tilt when absolute measures are
143 considered. The absence of between-gender differences when relative measures (standardized to the
144 orientation measured in sitting) are used further supports the possibility that this bias may be due to
145 anatomical factors, therefore constant throughout the task, although gender differences in trunk
146 orientation cannot be excluded from the current study. This gender-difference also highlights the need

147 to investigate the validity of absolute measures in a separate investigation in a laboratory setting.

148 Absolute measures were also less reliable than relative measures. This may be due to small differences
149 in smartphone position between days, since recent research shows that participant-placed sensor
150 positioning is less reliable than researcher-placed sensor positioning (Ruder et al., 2022). However,
151 similarly to what was discussed for the gender differences, the bias due to difference in smartphone
152 position would be removed by computing the relative orientation.

153 A strength of the current investigation lies in the simplicity of the experimental setup, which is a critical
154 factor for the potential implementation of smartphone measures in the clinic and for remote
155 assessment. Participants used their own smartphone, which implies that no specialized equipment had
156 to be bought or provided by the clinic. The app used in the current study can currently be used for free,
157 and the software used for data analysis is widely available. The choice of holding the smartphone on the
158 chest, while it may be difficult to implement in certain populations (see limitations below), removed the
159 need find a harness or other ways to secure the smartphone to the participant. Overall, this data
160 suggest that smartphone sensors are low-cost, widely available technology can be used to objectively
161 monitor how trunk orientation changes over time. Given the current emphasis on the use of wearables
162 in the assessment and treatment of individuals with low back pain (Hodges and van den Hoorn, 2022),
163 and recent evidence that patients may benefit from interventions addressing specific motor
164 impairments (Kent et al., 2015; van Dieën et al., 2018; van Dillen et al., 2021), future studies should
165 investigate whether smartphone sensors-based assessments may result in improved clinical outcomes.

166 This study also highlights some limitations of the technique that need to be addressed before it is
167 implemented in practice. First, validity of this measure compared to laboratory equipment, the smallest
168 number of trials that result in valid and reliable estimates, and whether there are differences between
169 smartphone brands and operating systems needs to be established. Second, this method allows only to
170 measure the orientation of the trunk in space, without differentiating motion at different spinal levels or

171 contribution of other joints, such as the hip. Whether it is possible to obtain kinematic measures
172 representative of lumbar motion, which has been reported to be impaired in individuals with low back
173 pain (Devecchi et al., 2021; Hooker et al., 2021; Laird et al., 2014), will need to be established in future
174 studies. Third, we could only assess the reliability of kinematics in the sagittal plane because
175 asymptomatic individuals have limited trunk motion in the frontal and transversal plane during sit-to-
176 stand, therefore the between-subject variance is too low to assess the reliability (de Vet et al., 2011). A
177 simpler app that shows the data directly on the screen and automatizes data analysis may also be easier
178 to implement in clinical practice. Finally, reliability may be lower when individuals have limited upper
179 limb function (e.g.: due to shoulder or hand injuries) or need to use the armrests to raise from the chair.

180 Our findings show that it is feasible to use smartphone sensors to measure sagittal trunk orientation
181 during sit-to-stand remotely in asymptomatic participants, and that these measures are reliable
182 between days. These measures may assist physiotherapists monitor remotely how trunk kinematics
183 changes over time in individuals with musculoskeletal disorders, and whether physiotherapy
184 interventions are effective interventions to modify trunk kinematics during sit-to-stand.

185

186 **CONFLICT OF INTEREST STATEMENT**

187 The authors declare no conflicts of interest.

188

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