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Oscillations in K(ATP) Conductance Drive Slow Calcium Oscillations in Pancreatic β-Cells 3

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33 Abstract

34 ATP-sensitive K^+ (K(ATP)) channels were first reported in the beta-cells of pancreatic 35 islets in 1984, and it was soon established that they are the primary means by which the blood 36 glucose level is transduced to cellular electrical activity and consequently insulin secretion. 37 However, the role that the K(ATP) channels play in driving the bursting electrical activity of islet 38 beta-cells, which drives pulsatile insulin secretion, remains unclear. One difficulty is that bursting 39 is abolished when several different ion channel types are blocked pharmacologically or genetically, 40 making it challenging to distinguish causation from correlation. Here, we demonstrate a means for 41 determining whether activity-dependent oscillations in K(ATP) conductance play the primary role 42 in driving electrical bursting in beta-cells. We use mathematical models to predict that if K(ATP) 43 is the driver, then, contrary to intuition, the mean, peak and nadir levels of ATP/ADP should be 44 invariant to changes in glucose within the concentration range that supports bursting. We test this 45 in islets using Perceval-HR to image oscillations in ATP/ADP. We find that mean, peak and nadir 46 levels are indeed approximately invariant, supporting the hypothesis that oscillations in K(ATP) 47 conductance are the main drivers of the slow bursting oscillations typically seen at stimulatory 48 glucose levels in mouse islets. In conclusion, we provide, for the first time, causal evidence for the 49 role of K(ATP) channels not only as the primary target for glucose regulation, but also for their 50 role in driving bursting electrical activity and pulsatile insulin secretion.

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- 52

53 Statement of Significance

Pancreatic beta-cells regulate blood glucose by secreting insulin in accordance with the glucose concentration. This metabolic sensing depends critically on ATP-dependent potassium channels, which link beta-cell fuel metabolism to the membrane potential. A key feature of this mechanism is the slow, five-minute oscillations observed in electrical activity, calcium, and metabolism. Mathematical models variously propose that oscillations in ATP/ADP either cause these oscillations or are just a consequence, as calcium influences both the production and consumption of ATP. We propose a novel way to test which is the case and confirm experimentally that ATP/ADP is the driver of beta-cell oscillations. Other proposed oscillation mechanisms in
contrast may mediate the faster oscillations that are also seen in beta-cells.

63

64 **Declaration of Interests**

65 The authors declare no competing interests

66

67 Introduction

68 Pancreatic β -cells are clustered together with other endocrine cells in the pancreatic islets 69 of Langerhans and are the sole insulin-secreting cells of the body. When blood glucose is low, β -70 cells are mostly inactive, but as glucose is increased so too is the cells' activity level (1). As a 71 result, the rate of release of insulin from β -cells increases in response to increases in the blood 72 glucose level. This is accomplished in two ways. In the first, primary pathway, β -cell electrical activity is increased at higher glucose levels, resulting in higher mean intracellular Ca^{2+} levels and. 73 subsequently, increased insulin secretion. A glucose amplification pathway builds on this primary 74 or 'triggering' pathway, and acts downstream of Ca^{2+} entry (2). The increased electrical activity 75 76 associated with increases in glucose is due to an increase in the ratio of ATP to ADP that is the direct result of glucose uptake and metabolism (1). ATP-sensitive K⁺ (K(ATP)) channels in the 77 78 plasma membrane are closed by ATP and opened by ADP, so the increase in ATP/ADP that results from glucose metabolism decreases the hyperpolarizing K(ATP) current ($I_{K(ATP)}$) thereby 79 80 depolarizing the cell (3-5).

81 In mouse islets, β -cells exhibit a robust bursting pattern over most of the stimulatory range of glucose, characterized by an active phase of electrical impulse generation followed by a silent 82 period during which the cell membrane is hyperpolarized. Sustained electrical oscillations in turn 83 result in oscillations in intracellular Ca^{2+} concentration: Ca^{2+} concentration is high during the burst 84 active phase when Ca²⁺ channels are open and while the cell is spiking and low during silent phases 85 86 when they are closed and spiking is suppressed (6). Since insulin exocytosis is driven by elevations in intracellular Ca^{2+} concentration, the oscillations in Ca^{2+} concentration produce concomitant 87 88 pulses of insulin secretion (7). A range of bursting patterns have been reported, including slow

bursting with periods of around 5 min, consistent with periods reported for pulsatile insulin release,
as well as fast bursting with periods of around 30 s or less.

91 What drives the slow bursting activity of β -cells? One hypothesis is that it results from 92 oscillations in the open/closed state of K(ATP) channels (8-11). In the simplest form of this 93 hypothesis, reduced K(ATP) conductance causes cells to depolarize and begins the active spiking phase of a burst. The spikes bring in Ca^{2+} , which activates Ca^{2+} pumps (12). The pumps consume 94 95 ATP (11), which allow some K(ATP) channels to reopen, terminating the spiking. Intracellular Ca²⁺ also increases dehydrogenase activity, increasing the production rate of ATP (13). The 96 97 oscillations in ATP/ADP that have been observed in MIN6 β -cells (14) and in β -cells in intact 98 islets are indeed consistent with this model (14,15). (For a discussion of how oscillations in 99 individual β -cells are coordinated by gap junctions see (16-20).)

100 However, even if bursting is driven by other mechanisms changes in intracellular Ca²⁺ 101 would affect ATP hydrolysis and dehydrogenase activity, and so still produce oscillations in 102 ATP/ADP. It is therefore hard to differentiate between cause and effect. Other mechanisms for electrical bursting have also been proposed, including cyclic activation of Ca²⁺-activated K⁺ 103 104 (K(Ca)) channels (21); current due to the activity of electrogenic ion pumps in the plasma 105 membrane (22,23); or a combination of various channels, pumps, and transporters (24). See (25) 106 for a review of models for bursting in β -cells. The difficulty of identifying the key mechanism 107 underlying bursting is that all of these, and other factors are known to oscillate in β -cells and may 108 therefore be correlated with bursting activity.

109 In principle, one could block one of these potential mediators, such as the K(ATP) channels 110 to determine if this interferes with the bursting rhythm. However, this may yield a misleading 111 result due to the complexity of the system. For example, while blocking K(ATP) channels is known 112 to reliably terminate the bursting pattern, blocking these channels removes most of the 113 hyperpolarizing current of the cell, putting the cell into a highly active state. Therefore, the bursting 114 might stop not because K(ATP) channel activity is no longer oscillatory, but because the 115 depolarization that results from channel blockade overwhelms the effects on membrane potential 116 of the true oscillatory mechanism.

We reasoned that what is needed is an approach that does not require artificial manipulation of any of the potential rhythmogenic factors. In this report, we demonstrate using mathematical modeling that monitoring changes in cytosolic ATP/ADP in response to changing glucose can 120 determine whether K(ATP) channel activity drives bursting in β -cells. Specifically, we 121 demonstrate that if oscillations in K(ATP) conductance are responsible for starting and stopping 122 bursts of electrical activity, then increases in glucose should have little or no effect on the mean, 123 peaks, or nadirs of ATP/ADP oscillations, provided that the cell is bursting. On the other hand, if 124 another mechanism drives bursting, such as (for example) K(Ca) channel current, then we predict 125 that the mean, peaks, and nadirs of ATP/ADP will increase with glucose rather than staying 126 constant.

127 To experimentally test this hypothesis we monitored the β -cell ATP/ADP ratio using the 128 fluorescent biosensor Perceval-HR (26) over a range of glucose concentrations where bursting 129 oscillations are observed. We also used the biosensor to examine the impact of interventions that 130 separately increase ATP consumption or production, since ATP/ADP reflects both processes. 131 Overall, we show that, contrary to intuition, mean, peak, and nadir ATP/ADP levels are nearly 132 constant over the range of glucose where islet β -cells exhibit bursting. With the aid of mathematical 133 modeling, we interpret this as direct evidence that slow bursting electrical oscillations in mouse 134 islet β -cells are driven by activity-dependent oscillations in the open/closed state of K(ATP) 135 channels.

136

137 Materials and Methods

138 Mathematical Model

139 The invariance of ATP/ADP peak, nadir, and mean values with changes in the stimulatory 140 glucose concentration is, as we demonstrate later, a property of a system in which the bursting 141 electrical activity requires oscillations in K(ATP) current that are driven by electrical activity-142 dependent changes in ATP/ADP. That is, changes in the current that are due to the intracellular Ca^{2+} level, which is high when the cell is in a burst active phase and low when in a silent phase. 143 144 To demonstrate this, we use two mathematical models: a simple mathematical model called the 145 phantom bursting model (PBM) (27), that contains a variable for the nucleotide ratio and a K(ATP) 146 current, among other currents, and a more complex one called the Integrated Oscillator Model 147 (IOM) that is described in detail in (28) and in the Supporting Material. This model has similar electrical and Ca²⁺ components, but more realistic K(ATP) current and a more detailed description
of the ATP dynamics that allows for intrinsic glycolytic oscillations.

150 Here we give a brief description of the elements of the PBM, which is employed in the 151 geometric demonstration for the mechanism underlying the ATP/ADP invariance phenomenon. 152 Fig. 1 provides a visualization of the PBM. The β -cell membrane potential is described by 153

$$\frac{dV}{dt} = -\frac{\left[I_{Ca} + I_{K} + I_{K(Ca)} + I_{K(ATP)}\right]}{C},\tag{1}$$

154

where I_{Ca} is an inward Ca²⁺ current, I_K is a delayed rectifying outward K⁺ current, $I_{K(Ca)}$ is a Ca²⁺activated K⁺ current, $I_{K(ATP)}$ is an ATP-sensitive K⁺ current, and *C* is the membrane capacitance. Activation of the Ca²⁺ current is assumed to be instantaneous with changes in voltage *V*. The activation variable for the delayed rectifier, *n*, is described by the first-order rate equation

$$\frac{dn}{dt} = \frac{n_{\infty}(V) - n}{\tau_n}.$$
(2)

160

161 The steady-state activation functions for the Ca^{2+} and delayed rectifier K⁺ channels, respectively, 162 are

$$m_{\infty}(V) = \frac{1}{1 + e^{(v_m - V)/s_m}},$$
(3)

$$n_{\infty}(V) = \frac{1}{1 + e^{(v_n - V)/s_n}}.$$
(4)

163 The K(Ca) channels are gated by the free cytosolic Ca^{2+} , with concentration *c*. This concentration 164 is increased by Ca^{2+} entering the cell through Ca^{2+} channels, and by Ca^{2+} entering the cytosol from 165 the endoplasmic reticulum (ER). The concentration is decreased by Ca^{2+} extrusion from the cell 166 by plasma membrane Ca^{2+} ATPase pumps (PMCA) and transported into the ER by Sarcoplasmic

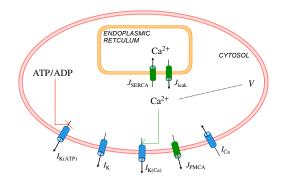


Figure 1: Illustration of the Phantom Bursting Model (PBM). The model contains modules for electrical activity and Ca^{2+} dynamics, and a variable for the nucleotide ratio ATP/ADP. *I*: currents, *J*: fluxes. K(ATP): ATP-sensitive K⁺ channels. K: delayed rectifier K⁺ channels. K(Ca): Ca²⁺-activated K⁺ channels. PMCA: plasma membrane Ca²⁺ ATPase. Ca: V-dependent Ca²⁺ current. SERCA: sarcoplasmic endoplasmic reticulum Ca²⁺ pumps. The red and green lines represent negative and positive feedback, respectively.

167 Endoplasmic Reticulum Ca^{2+} pumps (SERCA pumps). Thus, the cytosolic Ca^{2+} changes in time 168 according to

$$\frac{dc}{dt} = f_{\rm c}(J_{\rm mem} + J_{\rm ER}), \qquad (5)$$

169 where f_c is the fraction of cytosolic Ca²⁺ that is free and the membrane and ER Ca²⁺ fluxes are 170

$$J_{\rm mem} = -(\alpha I_{\rm Ca} + J_{\rm PMCA}), \qquad (6)$$

$$J_{\rm ER} = J_{\rm leak} - J_{\rm SERCA} , \qquad (7)$$

171 where α is a parameter, the flux of Ca²⁺ through the PMCA pumps (J_{PMCA}) is 172

$$J_{\rm PMCA} = k_{\rm PMCA} c , \qquad (8)$$

- 173 with parameter k_{PMCA} , and the leak of Ca²⁺ out of the ER (J_{leak}) and pumping of Ca²⁺ into the ER
- 174 through SERCA pumps (J_{SERCA}) are

$$J_{\text{leak}} = p_{\text{leak}}(c_{\text{ER}} - c) , \qquad (9)$$

$$J_{\text{SERCA}} = k_{\text{SERCA}}c , \qquad (10)$$

175 where p_{leak} and k_{SERCA} are parameters. The free Ca²⁺ concentration in the ER, c_{ER} , changes in 176 time according to

$$\frac{dc_{\rm ER}}{dt} = -f_{\rm ER}(V_c/V_{\rm ER})J_{\rm ER} , \qquad (11)$$

177 where f_{ER} is the fraction of free Ca²⁺ in the ER, and V_c , V_{ER} are the volumes of the cytosol and ER, 178 respectively.

The K(ATP) conductance is assumed to be increased in proportion to the ratio of the nucleotides ADP and ATP, a simplifying assumption but adequate for our purposes. In the model, the ratio a = ADP/ATP changes in time according to

182

$$\frac{da}{dt} = \frac{a_{\infty}(c) - a}{\tau_a},\tag{12}$$

183

184 where the steady-state function is an increasing sigmoid function of c,

185

$$a_{\infty}(c) = \frac{1}{1 + e^{(r-c)/s_a}},$$
(13)

186

187 with parameters τ_a and s_a . We interpret this equation as representing the increase of ATP 188 hydrolysis with calcium. The function *r* depends on the blood glucose concentration, *G*:

189

$$r = \frac{G - p_r}{K_r}.$$
(14)

190

191 In figures, we typically plot the ratio ATP/ADP = 1/a.

192 Finally, the ionic currents are:

193

$$I_{\rm Ca} = g_{\rm Ca} m_{\infty}(V)(V - V_{\rm Ca}) , \qquad (15)$$

$$I_{\rm K} = g_{\rm K} n (V - V_{\rm K}) \,, \tag{16}$$

$$I_{\rm K(Ca)} = g_{\rm K(Ca)}\omega(V - V_{\rm K}), \qquad (17)$$

$$I_{\mathrm{K}(\mathrm{ATP})} = g_{\mathrm{K}(\mathrm{ATP})} a(V - V_{\mathrm{K}}) , \qquad (18)$$

194

195 with $\omega = \frac{c^5}{c^5 + K_D^5}$. The values used for the conductance parameters, and all other parameters, are 196 given in Table 1. The full set of equations for the IOM is given in the Supporting Material. 197 Computer codes for both the PBM and the IOM are available for free download from 198 www.math.fsu.edu/~bertram/software/islet.

199

$g_{\rm Ca} = 1200 \ {\rm pS}$	$g_{\rm K} = 3000 {\rm pS}$	$g_{\mathrm{K(Ca)}} = 10 \mathrm{\ pS}$	$g_{\mathrm{K(ATP)}} = 500 \mathrm{pS}$
		C = 5300 fF	$\alpha = 4.5 \times 10^{-6} \text{ fA}^{-1}$
$V_{Ca} = 25 \text{ mV}$	$V_{\rm K} = -75 \text{ mV}$		μM ms ⁻¹
$\tau_n = 16 \text{ ms}$	$f_{\rm c} = 0.01$	$f_{\rm ER} = 0.01$	$k_{\rm PMCA} = 0.2 {\rm ms}^{-1}$
$K_D = 0.3 \ \mu M$	$v_n = -16 \text{ mV}$	$s_n = 5 \text{ mV}$	$v_m = -20 \text{ mV}$
$s_m = 12 \text{ mV}$	$k_{\rm PMCA} = 0.2 \ {\rm ms}^{-1}$	$k_{\text{SERCA}} = 0.4 \text{ ms}^{-1}$	$p_{\rm leak} = 0.0005 {\rm ms}^{-1}$
$V_{\rm c}/V_{\rm ER}=5$	$s_a = 0.1 \ \mu M$	$\tau_a = 300,000 \text{ ms}$	$p_r = 1.75 \text{ mM}$
$K_r = 58 \text{ mM}$			

Table 1: Parameter values used in the model.

200

201 Experimental Methods

202 Pancreatic islet isolation

Male Swiss-Webster mice (25-30 g) were euthanized in accord with the policies of the University of Michigan Institutional Animal Care and Use Committee (IACUC). The pancreatic bile duct was cannulated, allowing the pancreas to be inflated using a solution containing collagenase P (Roche Diagnostics, Indianapolis, IN). The pancreas was then isolated from the animal and digested further, allowing the islets to be freed from acinar tissue pancreas and handpicked, as described in (15). Individual islets were then transferred into RPMI1640 culture media
supplemented with FBS (10%), glutamine, and penicillin/streptomycin. Islets were kept in culture
in an air/CO₂ incubator at 37° C for three days (15).

211

212 Heterologous expression of the ATP/ADP reporter gene Perceval-HR and live cell imaging

213 A replication-deficient adenovirus was used to express the Perceval-HR biosensor into 214 pancreatic islet β -cells under the control of the rat insulin promoter to limit expression to β -cells 215 (15). Islets were placed in a glass-bottomed chamber (54 µl volume) (Warner Instruments/Harvard 216 Bioscience, Holliston, MA) on an Olympus IX71 inverted microscope equipped with a 20X/0.8 217 N.A. objective (Olympus, Melville, NY). The chamber was perifused at 0.3 ml/min and 218 temperature was maintained at 33°C using an inline solution and chamber heaters (Warner Instruments/Harvard Bioscience, Holliston, MA). Excitation light was provided by a TILL 219 220 Polychrome V monochromator (F.E.I., Munich, Germany). Excitation (x) or emission (m) filters 221 (Chroma Technology Corporation, Bellows Falls, VT) were used in combination with a 510lpxrxt 222 dichroic mirror as follows: 400/20x, 490/20x, and 535/30m. Fluorescence emission was collected 223 using a QuantEM:512SC camera (PhotoMetrics, Tucson, AZ) and excitation light was repeated 224 every six seconds. A single region of interest was used to quantify the average response of the β -225 cells using MetaFluor software (Molecular Devices, LLC, San Jose, CA) software.

226

227 Analysis of imaging data obtained using Perceval-HR

Statistical analysis was done using MATLAB. A linear mixed-effects model was fit using the MATLAB command fitlme to assess the dependence of the Perceval-HR fluorescence ratio on Time and Experiment. The model formula is: Ratio (493/403) ~ Time * Experiment + (1|Islet) + (1|Mouse), where the predictor Experiment corresponds to the different experimental protocols as described in Results. A further linear mixed-effects analysis was done to assess the dependence of the mean, amplitude, peak, and nadir values of Perceval-HR oscillations on Glucose in the case of bursting islets. The model formula is: Ratio (493/403) ~ Glucose + (1|Islet) + (1|Mouse). Details
of the results obtained are given in the Supporting Material.

236 **Results**

237 Mean ATP/ADP increases steadily with glucose concentration in models in which K(ATP) 238 channels are not the primary oscillatory mechanism

239 It has long been debated whether bursting electrical activity is driven by oscillations in 240 K(ATP) channel activity, or by another mechanism, with K(ATP) current simply setting the 241 threshold for the production of oscillations once the channels are closed by increased ATP/ADP. 242 Ideally, these two mechanisms could be distinguished by clamping K(ATP) conductance to its 243 mean value. If the oscillations in the K(ATP) conductance drive bursting, then clamping the 244 K(ATP) conductance should stop them. On the other hand, if other mechanisms mediate bursting, then preventing oscillations in K(ATP) conductance should not prevent oscillations in Ca²⁺ or 245 246 electrical bursting.

247 Two recent mathematical models of β -cell electrical activity are examples where bursting 248 occurs because of the combined activity of ion pumps, transporters, and ion channels rather than 249 due to K(ATP) conductance oscillations (24,29). We illustrate in Figs. 2A and B the predictions 250 of the models of Cha et al. (24) and Fridlyand et al. (29) and demonstrate how electrical oscillations 251 respond to clamping K(ATP) conductance to a fixed level at 3 min (as indicated by the arrow in 252 the figure) for these cases. In both models, bursting electrical activity can be seen to persist even 253 if oscillations in K(ATP) current are halted, highlighting the fact that these oscillations are not 254 essential to bursting; the mean contribution of K(ATP) current to the depolarization observed is 255 sufficient.

In contrast, as shown by the simulations depicted in Figs. 2C and D using the Integrated Oscillator Model (IOM) or the Phantom Bursting Model (PBM) in (27), respectively, bursting is abolished by clamping the K(ATP) conductance at 15 min (indicated by the arrow), demonstrating that in these models oscillations in K(ATP) are essential to the production of bursting.

260 While this intervention is straightforward to perform mathematically using a model, it is 261 considerably more difficult to do experimentally in islets. Therefore, we directed our attention to

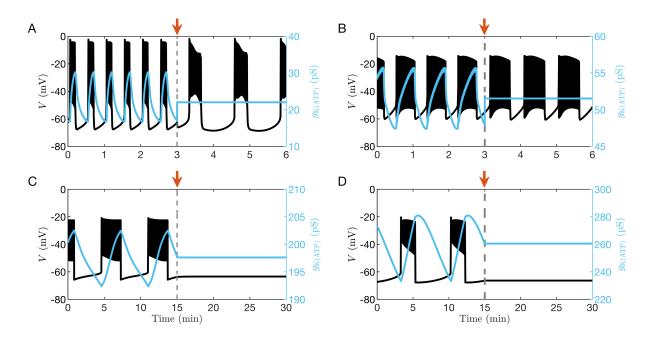


Figure 2: Model simulations in which the K(ATP) conductance is clamped at the arrow. The time courses are generated with (A) the Cha et al. model (24), (B) Fridlyand et al. model (29), (C) the IOM (28), and (D) the PBM (27). The clamped level of K(ATP) conductance is equal to the mean value of the preceding oscillations.

developing a simpler approach that does not rely on invasive interventions. Motivated by the
 importance of K(ATP) conductance oscillations described above, we instead focus on
 experimentally monitoring changes in nucleotide concentrations that occur in response to the
 application of a range of concentrations of glucose to isolated mouse islets.

266 As Cha et al. showed using their model (24), ATP increases and ADP decreases as glucose 267 concentration is increased. To demonstrate what happens when oscillations in K(ATP) channel 268 activity do not drive bursting, we used the Cha model to simulate the responses expected for two 269 different glucose concentrations, both of which result in electrical bursting. Fig. 3A shows 270 simulated oscillations in membrane potential (V) with the corresponding time course of ATP/ADP 271 superimposed. ATP/ADP can be observed to oscillate, declining during the burst active phase and 272 rising during its silent phase, as has been observed experimentally (14,15). Figs. 3B and C show 273 instead membrane potential and ATP/ADP oscillations obtained with two levels of glucose, with 274 only V traces shown (3B) or ATP/ADP (3C). Figure 3B shows that the duty cycle (the ratio of the

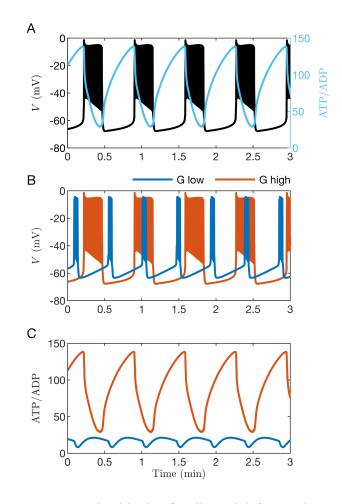


Figure 3: Time courses generated with the β -cell model from Cha et al. (24). (A) Bursting electrical activity with the ATP/ADP ratio superimposed. (B) Comparison of bursting at a lower glucose level (blue) and a higher level (orange). (C) The ratio of ATP to ADP increases when the glucose concentration is increased. For all panels, G = 7 mM and 11 mM for low and high stimulatory glucose, respectively.

active phase duration to the sum of the active and silent phase durations) is increased at the higher

276 glucose concentration relative to the lower one, in agreement with experimental studies (30).

Further, the ATP/ADP ratio is demonstrably larger at the higher vs. the lower glucose concentration; with peak, nadir, and mean levels all increasing with increased glucose (Fig. 3C).

The responses to glucose concentration as simulated using the Cha et al. (24) and Fridlyand et al. (29) models are summarized in Fig. 4. Here, both the duty cycle and the mean ATP/ADP ratio normalized to its largest value (<ATP/ADP>_n) are shown for glucose levels where the model

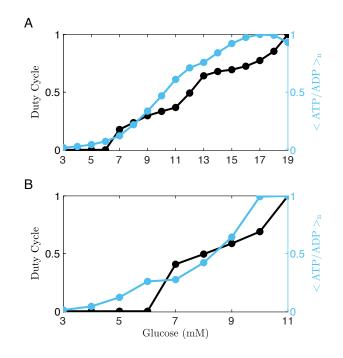


Figure 4: Quantification of duty cycle and normalized free ATP/ADP over a range of glucose levels. When the model cell is bursting, the mean value of ATP/ADP, <ATP/ADP>, is determined over one entire burst period (active phase plus silent phase). The normalization is performed by dividing <ATP/ADP> by its maximum over the full range of glucose concentrations. (A) Data from simulations of the Cha et al. model (24) show a monotonic increase in the normalized mean ATP/ADP level, <ATP/ADP>_n, as the glucose level is increased, with a dip to a slightly lower level at the last data point at which the cell enters a tonic spiking state. (B) Data from simulations of the Fridlyand et al. model (29) show a similar increase in <ATP/ADP>_n as the glucose concentration is increased and the cell is bursting, with a slight drop when the cell enters a tonic spiking state.

- cell is either silent (the lowest levels), bursting, or spiking tonically (the highest level). A duty cycle of 0 indicates that the model cell is silent, while a value of 1 means that it is tonically spiking.
- Values between 0 and 1 are obtained when the cell is bursting. In the case of bursting, mean
 ATP/ADP is computed over an entire burst period (the active plus silent phases).
- In simulations performed using either model, $\langle ATP/ADP \rangle_n$ increases at substimulatory glucose levels, when the model cell is silent, as has been shown experimentally (31). The rate of

289 increase in ATP/ADP is accelerated when the model cell enters the bursting state (e.g., duty cycle 290 > 0), and $\langle ATP/ADP \rangle_n$ continues to increase with glucose concentration at levels where the cell 291 is bursting. Only at the highest glucose level, when the model cell enters a tonic spiking state, does 292 $\langle ATP/ADP \rangle_n$ decline slightly, due to the increased ATP hydrolysis that drives Ca²⁺ pumping. 293 Overall, simulations carried out using either of these models predict a nearly monotonic increase 294 in $\langle ATP/ADP \rangle_n$ should be observed as glucose is increased and the model cell transitions from a 295 quiescent electrical state to bursting states with progressively increasing duty cycle. This behavior 296 is predicted for bursting that is predominantly driven by processes other than oscillations in 297 K(ATP) current (e.g., models where bursting persists despite clamping K(ATP) conductance to a 298 constant value, as in Fig. 2A, B).

299

300 Invariance in mean ATP/ADP ratio when oscillations in K(ATP) current drives bursting

301 We next wished to determine how ATP/ADP varies with glucose when oscillations in 302 K(ATP) conductance drive islet bursting. To do so, we examined responses to changing glucose 303 concentration using two mathematical models in which oscillations in K(ATP) conductance 304 mechanistically drive bursting. Figure 5 shows the counterpart of Fig. 3 for the IOM (left panels) 305 and for the PBM (right panels). In both models, the peak in ATP/ADP occurs at the beginning of 306 the active phase and its nadir occurs at the end of the active phase (Figs. 5A and B), as is also seen 307 using the model of Cha et al. The middle panels of the figure show the bursting patterns (V is 308 depicted) produced in response to two levels of glucose. The burst properties change as glucose is 309 raised; the active phases become longer, and the silent phase shorter, resulting in a larger duty 310 cycle at higher glucose. Also, the ATP/ADP ratio rises faster in the silent phase and declines more 311 slowly in the active phase when the glucose level is higher. This is a necessary consequence of the 312 increase in plateau fraction, provided that the peak ATP/ADP value occurs at the start of the active 313 phase and the nadir occurs at or near the end. That is the prediction of the IOM and the PBM (Fig. 314 5), but not consistently of the model of Cha et al. (Fig. 3), and is also in agreement with 315 experimental data (14,15). Yet, despite these changes, the peak and nadir levels of ATP/ADP are 316 the same at both glucose levels (Fig. 5E, F), as is mean ATP/ADP averaged over a burst period. 317 This "ATP/ADP invariance" is in striking contrast with the predictions of the other models, where 318 ATP/ADP rises steadily as glucose concentration is increased (Figs. 3, 4). In contrast, other aspects 319 of the observed time course do change with glucose, such as the rate of rise and fall of ATP/ADP

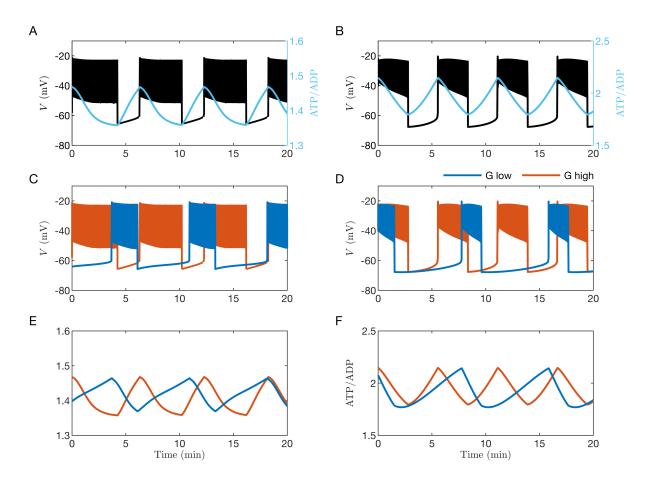


Figure 5: Simulations performed with the Integrated Oscillator Model (left panels) and the Phantom Bursting Model (right panels). (A, B) Bursting electrical activity with the ATP/ADP ratio superimposed. (C, D) Comparison of bursting at a lower glucose level (blue) and a higher level (orange). (E, F) Demonstration of invariance in the ATP/ADP peak, nadir, and mean at the two glucose levels. For both left and right panels, G = 8 mM and 13 mM for low and high stimulatory glucose, respectively.

320 (Fig. 5E). The reason for this invariance will be discussed later. The response of the IOM and the 321 PBM models to a range of glucose levels is quantified in Fig. 6. In both these cases, at 322 substimulatory levels of glucose (indicated by the 0 duty cycle), normalized ATP/ADP increases 323 as glucose concentration is increased, as we saw for the other mathematical models (Fig. 4). 324 However, unlike those models, normalized mean ATP/ADP is nearly flat over the range of glucose 325 concentration where the model cell exhibits bursting. When the cell enters a tonic spiking state 326 (duty cycle = 1), <ATP/ADP>_n declines, as was seen with the other models. The flat region shows

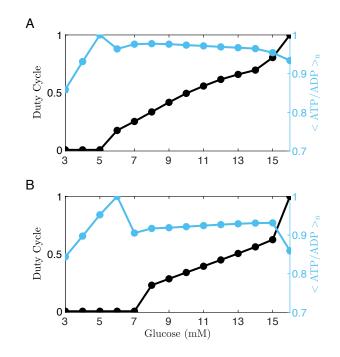


Figure 6: Quantification of duty cycle and ATP/ADP normalized over the range of values of glucose for the Integrated Oscillator Model (A) and the Phantom Bursting Model (B). The normalized ATP/ADP value $\langle ATP/ADP \rangle_n$ increases with increases in glucose concentration while the model cell is quiescent, but once the cell is busting $\langle ATP/ADP \rangle_n$ is invariant to changes in glucose concentration. When the cell enters a tonic spiking state there is a small decline in $\langle ATP/ADP \rangle_n$ due to ATP hydrolysis by Ca²⁺ pumps.

327 the ATP/ADP invariance property that was illustrated in Fig. 5. The lack of a rise in ATP/ADP 328 when glucose increases may seem counter to expectations, but it results from the fact that in the 329 model, increased production of ATP is balanced by increased consumption over the course of 330 each burst. This is discussed in more detail in a later section.

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Experimental measurements using a fluorescent biosensor show the ATP/ADP invariance predicted by the models

The model simulations shown thus far predict that if bursting is driven by oscillations in K(ATP) current, then the peak, nadir, and mean values of ATP/ADP should be invariant over the

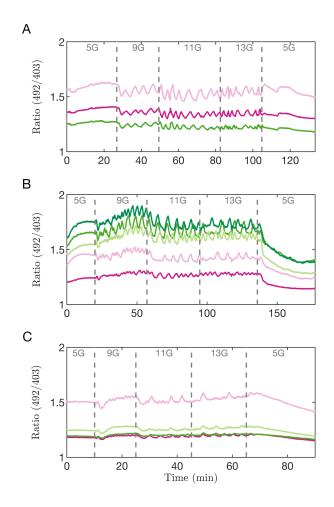


Figure 7: Measurements of Perceval-HR fluorescence ratio from 12 islets exposed to different glucose concentrations. Each panel corresponds to a different experiment from a Swiss-Webster mouse, and each trace to a different islet in which oscillations were present. For times when islets were bursting (9-13G) we observed no significant deviation of Ratio as a function of Time (*slope* = -5e-05 min⁻¹, *p*-value = 0.6; see Supporting Material).

range of glucose where bursting occurs. Alternatively, if bursting is driven by another mechanism, then we predict that invariance should not be observed. To test this prediction experimentally, we utilized the fluorescent biosensor Perceval-HR, which reports the ATP/ADP ratio selectively in islet β -cells (26). Islets were incubated in 5 mM glucose prior to increasing the concentration of glucose in steps, from 5, to 9, 11, 13, and finally back to 5 mM. In Fig. 7, the three panels shown depict Perceval-HR ratio measurements taken from islets of three different mice. In response to increasing the concentration of glucose from 5 to 9 mM, most islets exhibited an immediate drop of their fluorescence ratio (Fig. 7A and 7C). This same drop was observed with the model, as shown in Fig. 6. Our model suggests that this reflects an increase in ATP hydrolysis by the Ca²⁺ pumps of the plasma and ER membranes. At 5 mM glucose the islet is at rest and Ca²⁺ influx across the plasma membrane is consequently small. At 9 mM glucose, where islet β -cells are bursting, each burst brings Ca²⁺ into the cell which must in turn be pumped out. As a result, the Ca²⁺ pumps are more activated, and more ATP is correspondingly consumed.

350 For the three glucose levels where islets are bursting, we observed sawtooth-shaped 351 oscillations in the ATP/ADP ratio. We observed small oscillation-to-oscillation variations in the 352 patterns but not any systematic increase in ATP/ADP as glucose was increased (Experiment [1] in 353 the statistical analysis in Supporting Material; $slope = -5e-05 \text{ min}^{-1}$; p-value = 0.6). Indeed, the 354 peak, nadir, and mean levels we observed did not significantly increase over the range of glucose 355 levels where bursting is seen, as predicted by models where K(ATP) conductance oscillations drive bursting (change in peak Perceval-HR ratio per mM glucose: -0.00322 mM^{-1} , *p-value* = 0.0044; 356 357 nadir: -0.00158 mM^{-1} , *p-value* = 0.219; mean: -0.00339 mM^{-1} , *p-value* = 0.055; see Supporting 358 Material for details). The amplitude of oscillations also did not change significantly (-0.00164 mM⁻ ¹, *p*-value = 0.086). The data were therefore not compatible with the progressive increase in 359 360 ATP/ADP predicted by the alternative models where bursting is driven by a different mechanism 361 not involving K(ATP) oscillations, such as cyclic activation of K(Ca) channels or oscillatory ion 362 pump activity (Figs. 3, 4). This agreement with our model prediction supports the hypothesis that 363 the bursting oscillations of mouse islets are driven by oscillations in K(ATP) conductance, and again, our model suggests that increased ATP consumption during bursts prevents ATP/ADP from 364 365 increasing despite the increase in glucose.

When the glucose level was returned to 5 mM, all islets exhibited a decrease in fluorescence, sometimes following a transient increase (as in Fig. 7C). In all cases, the fluorescence level was observed to be lower in 5 mM at the end of the protocol than at the beginning. While more work is required to pin down the specific reason for this, our working hypothesis is that at higher glucose levels, the ER Ca²⁺ of bursting islets progressively increases due to increased cytosolic Ca²⁺ concentration driving ER Ca²⁺ loading. Once glucose is returned to 5 mM, however, Ca²⁺ drains from the ER into the cytosol, where it is pumped out of the cell by plasma membrane ATPases. This extra pumping action, not present initially when ATP/ADP was low, consumes
 more ATP thereby reducing ATP/ADP, and in turn reducing Perceval-HR fluorescence.

375

376 ATP/ADP invariance is lost when β -cells are prevented from bursting

377 In the data shown in Fig. 7 and the simulations produced using models of bursting driven 378 by K(ATP) oscillations (Figs. 5 and 6), invariance in mean ATP/ADP occurs only at glucose 379 concentrations where bursting is occurring. To further test this association, we examined how 380 ATP/ADP changed with glucose over the same concentration range but under conditions which 381 prevented bursting. Thus, we repeated the experimental protocol shown in Fig. 7, but now in the 382 presence of the K(ATP) channel activator diazoxide (Dz, 200 μ M) and elevated extracellular KCl 383 concentration (30 mM), a procedure widely used to clamp Ca²⁺ and voltage in β -cells (32). Dz was used to eliminate bursting at stimulatory glucose levels by pharmacologically opening K(ATP) 384 385 channels, and KCl was used to clamp the Ca²⁺ concentration to a level comparable to that observed in control islets exposed to stimulatory glucose. With Dz and KCl present at these levels, bursting 386 387 did not occur.

Figure 8A shows a simulation of this experiment carried out using the PBM. With each increase in glucose concentration (shown by the arrows), ATP/ADP is predicted to increase. This is because while ATP production increases with glucose, the presence of Dz and KCl clamp Ca^{2+} to a fixed level, preventing a countervailing increase in ATP consumption due to bursting and allowing production to dominate.

393 This was tested experimentally using Perceval-HR to measure ATP/ADP (Fig. 8B, C). 394 When the glucose concentration was increased from 5 to 9 mM in the presence of 200 μ M Dz, the 395 large drop of the florescence ratio typically seen (see Fig. 7) was no longer present. Instead, the 396 ratio can be seen to rise in this case. As the glucose level was increased further, the ratio continued 397 to increase (Experiment [2] in the statistical analysis in Supporting Material; $slope = 0.0021 \text{ min}^{-1}$ 398 ¹; *p-value* < 0.001). This monotonic increase confirmed the prediction of the model. Our 399 interpretation is that the increase in ATP production was not offset by an increase in ATP 400 consumption (as when islets are bursting) due to the clamping of cytosolic Ca²⁺ and thus a constant 401 level of ATP consumption.

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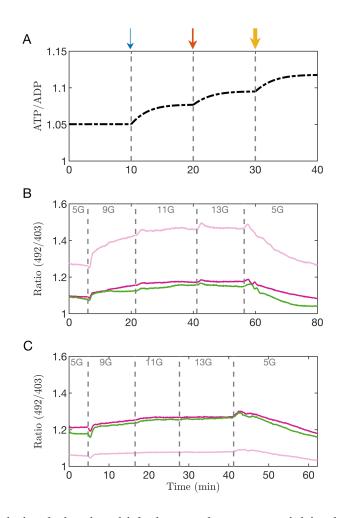


Figure 8: (A) Model simulation in which the membrane potential is clamped with diazoxide (Dz) and elevated KCl. Glucose concentration is increased at the arrows, from G = 5 mM to 9 mM, from 9 mM to 11 mM, and finally to 13 mM. The width of each arrow indicates the size of the glucose concentration. (B, C) Two experiments in which islets were exposed to Dz (200 μ M) and KCl (30 mM) and in which glucose was increased from 5 mM to higher levels, as indicated, before being returned to 5 mM. Each trace corresponds to an islet, and is representative of the protocol applied to 21 islets isolated from 2 different Swiss-Webster mice from 6 different sets of recording sessions. During the time interval where glucose concentrations were increased, we observed a significant positive slope in ratio vs time (*slope* = 0.0021 min⁻¹; *p*-value < 0.001).

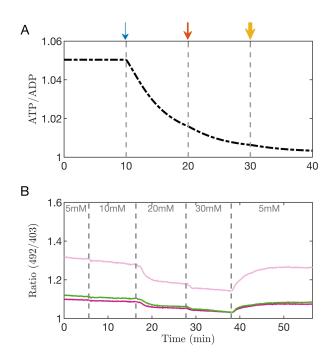


Figure 9: (A) Model simulation in which the membrane potential is clamped with diazoxide (Dz) and low glucose (G = 5 mM), and application of KCl was simulated by changing the K⁺ Nernst potential. At the first arrow $V_K = -60 \text{ mV}$, at the second $V_K = -50 \text{ mV}$, and at the third $V_K = -40 \text{ mV}$. (B) Experiment in which islets were exposed to Dz (200μ M) and 5 mM glucose, and in which the KCl concentration was increased in steps, as indicated, before being returned to 5 mM. Each trace corresponds to an islet, and is representative of the protocol applied to 22 islets isolated from 4 different Swiss-Webster mice from 6 different sets of recording sessions. During the time interval where KCl concentrations were increased, we observed a significant positive slope in Ratio vs Time (*slope* = -0.0033 min⁻¹; *p*-value < 0.001).

404

405 ATP/ADP declines when ATP consumption is increased

406 To test whether increasing ATP consumption while keeping production constant causes 407 ATP/ADP to decrease Dz was again used to inhibit electrical bursting, but this time the glucose 408 level was kept constant (5 mM), and we sequentially increased the extracellular KCl concentration 409 instead to stimulate Ca^{2+} entry. A model simulation of this experiment is shown in Fig. 9A, where 410 the K⁺ Nernst potential (V_K) was increased at the time points denoted by the arrows, simulating

- 411 the effects of stepwise increases in KCl concentration. The result of increasing V_K is to depolarize
- 412 the cell membrane, opening Ca^{2+} channels and bringing more Ca^{2+} into the cell. This Ca^{2+} must
- 413 then be pumped out and the increased hydrolysis of ATP needed to power the Ca^{2+} pumps to do
- 414 this results in a decline in ATP/ADP.

To test this prediction experimentally, islets were exposed to Dz and to increasing levels of KCl, with glucose held constant at 5 mM (Fig. 9B). In each of the islets, an increase in KCl concentration resulted in a corresponding drop in Perceval-HR fluorescence. Thus, depolarizing the cell and increasing Ca^{2+} influx resulted in a net drop in ATP/ADP (Experiment [3] in the statistical analysis in Supporting Material; *slope* = -0.0033 min⁻¹; *p-value* < 0.001), as predicted by the model. Our interpretation here is that increased ATP hydrolysis is necessary to power Ca^{2+} pumping due to the presence of KCl (11), increasing ATP demand.

422

423 A mechanism for the ATP/ADP invariance seen when bursting is driven by K(ATP) 424 conductance

Why is the mean ATP/ADP level invariant over the range of glucose levels at which the cell is bursting when the bursting is driven by K(ATP) current oscillations? The previous section suggests that this happens because the production and consumption of ATP by the cell are balanced during each oscillation cycle, but not when oscillations are absent.

429 To understand this in greater depth, we used a mathematical approach called fast-slow 430 analysis, applied to the PBM used to demonstrate invariance in Figs. 5B and 6B. In fast-slow 431 analysis, first introduced to the analysis of β -cell bursting by Rinzel (33,34), model variables are 432 partitioned into those that change rapidly and those that change slowly during bursting. The 433 subsystem of fast variables is then analyzed while treating the slow variables as slowly-varying 434 parameters. In our case, membrane potential (V), the activation of delayed rectifier K⁺ channels (*n*), and free cytosolic Ca^{2+} concentration (*c*) are all fast variables. The Ca^{2+} concentration of the 435 436 endoplasmic reticulum (c_{ER}) and the ATP/ADP ratio (1/a) are slow variables. The long-term 437 behavior of the three-dimensional fast subsystem is characterized as a bifurcation diagram, as shown in Fig. 10. Here, the slow variable c_{ER} is fixed at the value it takes on at the beginning of a 438 439 burst active phase to focus on the more important changes in ATP/ADP. At each value of 440 ATP/ADP the long-term behavior of the fast subsystem is shown, using V as a readout.

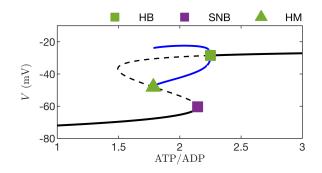


Figure 10: Bifurcation diagram of the fast subsystem (*V*, *n*, and *c*) of the model used in Figs. 5B and 6B. The slow variable c_{ER} is held fixed at the value it takes on at the beginning of a burst active phase, $c_{\text{ER}} = 51 \,\mu\text{M}$. The maximal K(Ca) conductance parameter is $g_{K(Ca)} = 10 \,\text{pS}$. The black curves represent resting or stationary solutions; solid portions represent stable solutions and dashed portions represent unstable solutions. The two blue curves represent periodic tonic spiking solutions; points on the bottom curve are spike minima and points on the top curve are spike maxima. There are three bifurcation points: HB=Hopf bifurcation from which the periodic branch emerges, SNB=saddle-node bifurcation where stable and unstable stationary solutions coalesce, and HM=homoclinic bifurcation.

441 At low values of ATP/ADP, K(ATP) channels are largely activated, providing 442 hyperpolarizing current that pins the cell to a negative resting state, near -70 mV. This is illustrated 443 by the left portion of Fig. 10; each point on the solid black curve represents the resting V value at 444 the corresponding value of ATP/ADP. At the other extreme, when ATP/ADP is large, the K(ATP) 445 channels are mostly closed, which greatly reduces the magnitude of the hyperpolarizing current. 446 This puts the model cell into another resting state, but this time at a voltage near -30 mV. This is 447 the case shown in the right portion of Fig. 10, where again the solid black curve is a curve of 448 resting or "stationary" states. Between these extremes, the fast subsystem has two co-existing 449 stable behaviors. One is a hyperpolarized steady state (points on the bottom solid black curve), 450 while the other is a periodic solution that corresponds to the spikes during a burst. This periodic 451 solution reflects spiking, with the minimum voltage of the action potential shown as a point on the 452 bottom blue curve in Fig. 10, and the maximum voltage shown as a point in the top blue curve. 453 Thus, for any fixed value of ATP/ADP between the green triangle (a homoclinic bifurcation, HM) 454 and the green square markers (a Hopf bifurcation, HB), the fast subsystem can produce spiking.

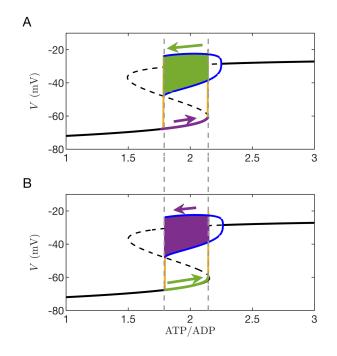


Figure 11: ATP/ADP invariance explained through a fast-slow analysis. The arrows indicate direction and relative magnitude of motion. (A) The burst trajectory is projected into the plane of the ATP/ADP and *V* variables. The silent-to-active transition (rightmost dashed vertical line) occurs at the knee of the s-shaped bifurcation diagram (the saddle-node bifurcation), while the active-to-silent transition (leftmost dashed vertical line) occurs at the termination of the periodic spiking branch (the homoclinic bifurcation). The glucose concentration is *G* = 8 mM. The color coding is purple=slow motion, green=fast motion, yellow=very fast motion (B) When the glucose level is increased to *G* = 13 mM the burst trajectory covers the same path along the fast subsystem bifurcation diagram. For this reason, the peak, nadir, and mean values of ATP/ADP are the same at both glucose levels. The only difference is the speed at which the trajectory moves through the silent phase and the active phase of the burst. In both (A) and (B), $g_{K(Ca)} = 10 \text{ pS}$.

However, between the green triangle and the purple square (a saddle-node bifurcation, SNB), the
fast subsystem can also be quiescent. The system is therefore bistable over this parameter interval.
The dashed curves in the figure represent unstable equilibria, where the system cannot rest but
which influence its behavior.

The next step in the fast-slow analysis is to superimpose the bursting trajectory onto the fast-subsystem bifurcation diagram, as is shown in Fig. 11. During the start of the silent phase 461 (Fig. 11A), the system trajectory (purple) moves from left-to-right along the bottom stationary

462 branch. The left-to-right motion occurs because the Ca^{2+} concentration is low and little ATP

hydrolysis is needed to power the Ca²⁺ pumps, so ATP/ADP increases due to glucose metabolism 463 464 (this is also observed in Fig. 5A). Once the trajectory reaches the rightmost dashed vertical line, 465 which indicates the end of the lower stationary branch, it rapidly moves to the spiking branch, starting a burst active phase (green). The subsequent spiking that ensues brings Ca^{2+} into the cell, 466 and ATP is consumed as Ca²⁺ pumps work to remove it. As a result, ATP/ADP declines and the 467 468 trajectory moves leftward along the periodic branch until its termination point (the leftmost dashed 469 vertical line). From here the trajectory returns to the bottom stationary branch, ending the active 470 phase and starting the next silent phase.

471 The peak ATP/ADP during bursting is the value at the silent-to-active phase transition (the rightmost dashed curve). Here, the conductance of K(ATP) current ($g_{K(ATP)}$; Eq. 18) is sufficiently 472 473 small that the cell escapes from the resting state and begins spiking. The nadir of ATP/ADP is the 474 value at which the active-to-silent transition occurs (the leftmost dashed curve). Here, $g_{K(ATP)}$ is 475 so large that the hyperpolarizing K(ATP) current stops the cell from spiking. These critical values 476 are the same for any glucose level for which the cell bursts because it always takes the same amount 477 of K(ATP) conductance to start or stop a burst active phase. The only thing that changes when the 478 glucose level is changed is the rate at which ATP/ADP changes, i.e., the rate at which the trajectory 479 travels rightward along the lower stationary branch (due to net ATP production) or leftward along the upper spiking branch (due to net ATP utilization). At lower glucose levels with lower ATP 480 481 synthesis, the trajectory moves slowly (color coded as purple with short purple arrow) along the 482 bottom stationary branch and rapidly (color coded as green with long arrow) along the spiking 483 branch, so the duty cycle is near 0. At higher glucose levels with greater ATP synthesis, the 484 trajectory moves rapidly along the stationary branch and slowly along the spiking branch, so the 485 duty cycle is near 1. However, the peak and nadir levels of ATP/ADP, as well as mean ATP/ADP, 486 are all invariant since the amount of K(ATP) conductance needed to start or stop the burst active 487 phase is always the same (assuming that glucose has no direct effect on ion channels). This is 488 demonstrated in Fig. 11B, which shows the fast-subsystem bifurcation diagram and the 489 superimposed burst trajectory at a higher glucose level. This panel looks similar to panel A. All 490 that has changed is how rapidly the trajectory moves along portions of the bifurcation diagram. 491 Motion during the silent phase is fast (green with long arrow), while motion during the active

492 phase is slow (purple with short arrow). In this model, as long as the cell is bursting, changes in 493 glucose will have no effect on the ATP/ADP peak, nadir, or mean values. This is the basis for the 494 ATP/ADP invariance property observed in Figs. 5 and 6, and our experimental findings support 495 this mechanism for invariance of mean, peak, and nadir ATP/ADP with changes in the glucose 496 concentration.

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499 ATP/ADP invariance is lost when other currents contribute to drive the bursting

500 We now consider the case where oscillations in K(ATP) current are not the prime driver of 501 bursting. This is the case in fast bursting, where variations in K(Ca) conductance or some other 502 process initiate and terminate bursts of β -cell spikes (24,27,35,36). In Fig. 4 we showed that in 503 such a case the invariance we observed for the ATP/ADP nadir, peak, and mean values is lost. In 504 Fig. 12 we demonstrate why this is the case. The figure was made using the PBM, which produces 505 slow bursting driven almost entirely by variation in K(ATP) current when the K(Ca) conductance 506 is low, and faster bursting driven primarily by variation in K(Ca) current when its conductance is 507 high (27). The bursting is shown projected into two different planes, both with ATP/ADP on the x-axis. In the V vs. ATP/ADP plane (Fig. 12A), with a small K(Ca) conductance ($g_{K(Ca)} = 10 \text{ pS}$) 508 509 the slow bursting trajectory is almost the same when G = 8 mM (black curve) and when G = 13510 mM (gray), for the reasons described above and in Fig. 11. That is, the SNB and HM bifurcations 511 that start and stop each burst active phase are nearly the same at both glucose levels, so the nadir, 512 peak, and mean ATP/ADP values are invariant to changes in glucose. With the faster bursting (period ~2 min when G = 11 mM) produced with a larger K(Ca) conductance ($g_{K(Ca)} = 300$ pS), 513 514 the projected burst trajectory is very different at the two different glucose concentrations. When 515 the glucose concentration is increased from 8 mM (blue curve) to 13 mM (cyan curve) the burst 516 trajectory is shifted rightward. This rightward shift results in an increase in the nadir, peak, and 517 mean ATP/ADP levels. In this case, the SNB and HM bifurcations that start and stop each burst 518 are right shifted.

519 What is responsible for these differences between the low and high values of $g_{K(Ca)}$? As 520 described in the previous section, in the case of low $g_{K(Ca)}$, the primary intracellular variable 521 controlling the transitions between active and silent phases is ATP/ADP. However, $g_{K(Ca)}$ still

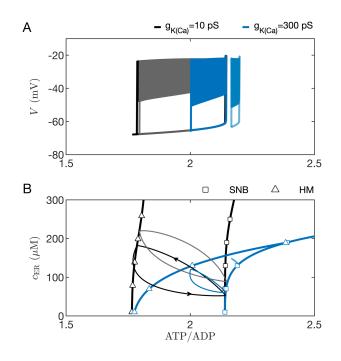


Figure 12: In simulations with the PBM, ATP/ADP invariance to changes in glucose is lost when $g_{K(Ca)}$ is increased from 10 pS, which yields slow bursting (period ~6 min) driven by K(ATP) current, to 300 pS, which yields faster bursting driven mainly by K(Ca) current (period ~2 min). (A) Simulated slow bursting trajectory with G = 8 mM (black) and G = 13 mM (gray) glucose projected into the *V* vs. ATP/ADP plane. The projections are nearly identical, in contrast to the case with faster bursting, where the trajectory corresponding to G = 8 mM (blue) is to the left of that corresponding to G = 13 mM (cyan). (B) Curves of saddle node bifurcations (SNB) and homoclinic bifurcations (HM) in the c_{ER} vs. ATP/ADP plane are identified using squares and triangles, respectively. The black curves correspond to slow bursting, while the blue correspond to faster bursting. Also shown are projections of slow bursting at 8 mM and 13 mM glucose (black and gray loops, respectively) and of the faster bursting at 8 mM and 13 mM

522 contributes but to a very small degree; even large, burst-driven changes in intracellular Ca²⁺ 523 activate only a small K(Ca) current. On the other hand, when $g_{K(Ca)}$ is larger, the K(Ca) current 524 can contribute significantly to burst initiation and termination, with Ca²⁺ entry and movement in 525 and out of the ER taking on a more central role. The slow filling of the ER slows the rise of $g_{K(Ca)}$ 526 during the active phase, and the slow emptying of the ER slows the fall of $g_{K(Ca)}$ during the silent 527 phase (27).

528 The shift in the two bifurcations can be viewed in the plane of c_{ER} and the ATP/ADP 529 concentration (Fig. 12B), as was done in an earlier analysis (37). This plane is used to illustrate 530 the shift in bifurcations because the range of c_{ER} values covered during bursting is different for fast 531 and slow bursting, and for different glucose levels. For each value of $g_{\text{K}(\text{Ca})}$ and *G* the trajectory 532 of c_{ER} and ATP/ADP forms a closed loop.

533 The active phase starts when the trajectory reaches the curve of SNB bifurcations (black 534 squares) and ends when it reaches the curve of HM bifurcations (black triangles). Both bifurcation 535 curves are nearly vertical, indicating that their ATP/ADP values do not vary much with changes 536 in the glucose level. Indeed, at higher glucose levels the burst trajectory is shifted upward (gray 537 loop), but the ATP/ADP values that bound it on the left and right change little. In contrast, during 538 fast bursting, both the HM and SNB curves bend dramatically rightward (blue curves with blue 539 triangles and squares), becoming nearly horizontal. This indicates that an increase in the glucose 540 level dramatically shifts the ATP/ADP levels at which burst active phases start and stop. Indeed, 541 the projected fast burst trajectory is far to the right at a high glucose concentration (cyan curve, 542 G = 13 mM) compared to the case of a lower glucose concentration (blue curve, G = 8 mM).

543 We quantify the progressive loss of invariance that occurs as control of bursting is shifted 544 from K(ATP) current to K(Ca) current in Fig. 13, using the PBM as well as the more complex 545 IOM model. In both models, fast bursting is produced by increasing the value of the K(Ca)

conductance ($g_{K(Ca)}$). Figure 13 shows the duty cycle and $\langle ATP/ADP \rangle_n$ over a range of values of 546 glucose for three values of $g_{K(Ca)}$ for the IOM (left panels) and the PBM (right panels). The black 547 548 curves represent the slow bursting (period $\sim 6 \text{ min}$) analyzed in Fig. 6, while the orange curves 549 illustrate the results obtained for fast bursting (period ≤ 20 sec). For each curve, the slope averaged 550 over the range of glucose values that produced bursting was calculated by fitting straight lines using least squares and is plotted as a bar graph in the inset. The slope of the normalized ATP/ADP 551 552 curves increases with higher values of $g_{K(Ca)}$ for both the IOM (panel A) and the PBM (panel B). 553 That is, the invariance in the mean ATP/ADP value with changes in glucose is progressively lost 554 as the role of K(Ca) current in driving bursting is increased.

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557 **Discussion**

558 We have proposed a novel approach for determining whether bursting electrical activity in 559 pancreatic β -cells is driven by activity-dependent oscillations in K(ATP) current. This method 560 requires only that ATP/ADP be monitored in the islet at different glucose concentrations for which 561 the islet cells are bursting. If there is invariance in the peak, nadir, and mean of ATP/ADP during 562 the oscillations, then K(ATP) channels drive bursting. If there is no invariance, then K(ATP) 563 channels alone do not drive bursting but would still help to set the level of depolarization of the 564 membrane and the threshold where oscillations begin. We demonstrated these points using 565 mathematical models (Figs. 3, 4, 5, 6), and verified ATP invariance using the fluorescent probe 566 Perceval-HR to monitor the ATP/ADP level of single islets (Fig. 7). Such invariance does not occur at subthreshold glucose concentrations (14,31), or at stimulatory glucose levels when 567 568 bursting is prevented by activating K(ATP) channels pharmacologically with diazoxide. Indeed, 569 experiments where we blocked bursting demonstrated that increasing ATP production by 570 increasing the glucose concentration resulted in an increase in the ATP/ADP ratio (Fig. 8), while increasing ATP utilization by depolarizing the cell and raising the intracellular Ca²⁺ level resulted 571 572 in a decrease in the ATP/ADP ratio (Fig. 9). These data match predictions generated by the PBM 573 and the IOM, but also match predictions from other β -cell models which differ from ours primarily 574 in the mechanism for bursting (22,24).

575 Although the ATP/ADP invariance property may seem counterintuitive, it has appeared in 576 two previous studies, but its significance and implications for the mechanism of bursting were not 577 explored (Fig. 3 of (14), Fig. 3 of (38)). In (14), the submembrane ATP/ADP level was measured 578 with Perceval fluorescence, and in one islet recording it appears that the mean level was invariant 579 over a glucose range of 9 to 20 mM (the regions where oscillations were evident). The invariance 580 of peak and nadir values is not as evident, and it appears that the amplitude of the oscillations may 581 grow with the glucose level. However, this was not quantified, and there appears to be significant 582 burst-to-burst heterogeneity in oscillation amplitude for a single glucose level.

It is natural to assume that ATP/ADP should increase when glucose is raised from one level to a higher level, as suggested in a recent review (1), since ATP production increases with glucose. Indeed, several studies showed an increase in islet ATP content or ATP/ADP ratio at higher glucose levels. However, in these studies no comparison was made between ATP/ADP at different

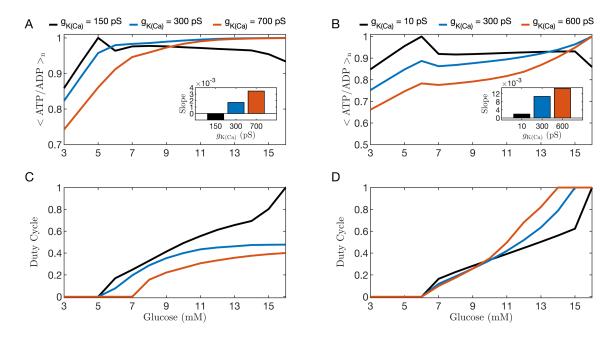


Figure 13: Quantification of the mean normalized ATP/ADP ratio (A, B) and duty cycle (C, D) over the range of values of glucose for three different values of $g_{K(Ca)}$ (color coded). The curves were generated with the Integrated Oscillator Model (left column) and the Phantom Bursting Model (right column). The black curve shows the results for slow bursting (as in Fig. 6). At 11 mM glucose, the bursting simulated with the IOM (A, C) has a period of ~6 min for $g_{K(Ca)} = 150 \text{ pS}$ (black curves), ~2 min for $g_{K(Ca)} = 300 \text{ pS}$ (blue curves) and ~9 sec for $g_{K(Ca)} = 700 \text{ pS}$ (orange curves). The PBM (B, D) has a period of ~6 min for $g_{K(Ca)} = 10 \text{ pS}$ (black curves), ~2 min for $g_{K(Ca)} = 300 \text{ pS}$ (blue curves) and ~20 sec for $g_{K(Ca)} = 600 \text{ pS}$ (orange curves). For each curve, the slope averaged over the range of glucose values that produced bursting was calculated using linear least squares fitting and is plotted as a bar graph in the insets to the top panels.

glucose levels at which the islet was bursting. For example, in one study most of the data points were obtained at basal glucose (Fig. 3 of (31)) and only one data point (at 10 mM glucose) likely corresponded to a bursting islet. At the basal levels, the ATP concentration increased with the glucose concentration, as predicted in our model simulations with the IOM and the PBM (Fig. 6). In another study, comparison was made at a very low glucose level (3 mM) when the β -cells would be electrically silent and at a very high glucose level (17 mM) when they would most likely be continuously spiking (39). In two other studies, batches of islets were averaged and it was not
determined whether they were silent, bursting, or continuously spiking (Fig. 2 of (11), Fig. 5 of
(40)).

During bursting, the Ca^{2+} level is increased during each active phase, and the increased 596 597 level results in increased ATP consumption to power Ca^{2+} pumps (11). With the longer duty cycles 598 associated with higher glucose levels this consumption is greater, so even though ATP production 599 is higher, so is ATP consumption. When an islet is bursting, these two effects exactly balance over 600 the course of a complete active/silent cycle. We illustrated this using fast-slow analysis (Figs. 10 601 and 11), where the essence of the argument is that if activity-dependent oscillations in K(ATP) 602 channels alone drive bursting, then a burst active phase starts when ATP/ADP is sufficiently high 603 (so the K(ATP) conductance is sufficiently low) and stops when ATP/ADP is sufficiently low (so 604 the K(ATP) conductance is sufficiently high). The glucose level only determines how fast 605 ATP/ADP rises and falls, which determines the duty cycle, but does not change the ATP/ADP or $g_{\rm K(ATP)}$ levels required to start/stop burst active phases. 606

It is often the case that the details of a mathematical model, such as specific values of 607 608 parameters chosen, have a large effect on the behavior of the model. Fortunately, that is not the 609 case with the invariance in mean ATP/ADP. Any β -cell model in which the bursting is driven by 610 oscillations in the K(ATP) current would exhibit invariance in the ATP/ADP peaks, nadir, and 611 mean. We demonstrated this using two different models in Figs. 5, 6. Indeed, this universality 612 (illustrated in the fast-slow analysis of Figs. 11and 12) is precisely why ATP/ADP invariance 613 implies that oscillations in K(ATP) current drives the bursting. In contrast, invariance in the mean 614 ATP/ADP level would not be expected if bursting was driven by a mechanism other than 615 oscillations in K(ATP) conductance (Figs. 3, 4). In this case, the initiation and termination points 616 of a burst active phase are set largely by conductances that do not depend on ATP/ADP, so no 617 constraint is imposed on the level of K(ATP) conductance, nor consequently the peaks and nadirs 618 of the oscillating ATP/ADP levels.

619 If a different channel other than K(ATP) drives bursting, and the activation/inactivation 620 variable for that current were a target of glucose, then that variable would exhibit invariance, rather 621 than ATP/ADP. As a demonstration of this, and that history indeed seems to repeat itself, this 622 invariance argument was used by Himmel et al. in 1987 as evidence against Ca²⁺-activated K⁺ 623 current (K(Ca) current) as being the mechanism for bursting in β-cells Himmel and Chay (41). It 624 had been proposed earlier by Chay and Keizer that K(Ca) channels drive bursting and that glucose acts by increasing the Ca^{2+} pump rate (21,42). That model predicted that cytosolic Ca^{2+} would rise 625 626 and fall during bursting in a sawtooth manner, as for the ATP/ADP ratio used here (Fig. 5). 627 Increasing the pump rate indeed increased the duty cycle in the original Chay-Keizer model, as desired, but as pointed out in (41), it had no effect on the mean intracellular Ca^{2+} concentration. 628 Since an increase in mean intracellular Ca²⁺ is one factor responsible for triggering glucose-629 dependent insulin secretion, the Ca²⁺ invariance clearly conflicted with the data and therefore 630 argued against the assumption that K(Ca) current drives bursting or that the Ca²⁺ pump rate is 631 632 glucose-dependent, or both. Both assumptions turned out to be incorrect.

633 Throughout the article, our main focus has been on "slow bursting", which is bursting that 634 exhibits a period of several minutes. However, mouse islets also exhibit a faster form of bursting 635 having a period of 30 sec or less (43). It is almost certain that the mechanism for this "fast bursting" 636 is different from that of slow bursting, and is likely driven at least in part by K(Ca) conductance, 637 as originally proposed (21,42). For this fast bursting, then, we showed that increasing glucose from 638 one stimulatory level to another would increase ATP/ADP (Fig. 13). More generally, the models 639 (27,44) predict that as burst period varies from slow to fast, K(Ca) channels would play an 640 increasingly large role while K(ATP) channels become progressively less important. We have 641 found in model simulations that the slope of the ATP/ADP ratio vs. glucose curve within the burst 642 increases continuously from 0 as the burst period decreases. Thus, others trying to replicate our 643 findings may obtain a range of possible results, depending on the period of the oscillations in their 644 islet preparations. Similarly, the invariance property would not hold if multiple currents work together to drive bursting if K(ATP) channels play only a minor role, as in (24,29), as we 645 646 demonstrated in Figs. 3 and 4. Therefore, the ATP/ADP invariance is quite unusual, but also very 647 informative, since it indicates both that for the slowest range of burst periods, K(ATP) current 648 drives bursting and that the target of glucose is the nucleotide ratio.

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651 Conclusion

652 We used mathematical models to predict that if oscillations in K(ATP) channel conductance drive the slow Ca²⁺ oscillations of pancreatic β -cells, then ATP/ADP should exhibit invariance over 653 glucose concentrations that support bursting. Our confirmation of this prediction supports the 654 conclusion that K(ATP) channels are the primary drivers of slow Ca^{2+} oscillations and not merely 655 passive followers of Ca²⁺-mediated changes in metabolism. The model indicates that this is the 656 case because during oscillations, glucose-induced increases in mean Ca²⁺ due to increased ATP 657 production are balanced by increased ATP consumption to pump Ca²⁺. We supported this 658 659 interpretation experimentally by showing that when glucose is increased but Ca²⁺ is clamped, ATP/ADP rises, whereas if glucose is fixed and Ca^{2+} is increased, ATP/ADP falls. 660

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662 Author Contributions

All authors contributed to the conceptualization of the project, the experimental design, and the writing and editing of the manuscript. I.M. performed mathematical simulations and analysis and the statistical analysis, B.M.T. and V.P. carried out experiments, L.G.-G., A.S.S., L.S.S. and R.B. provided resources and supervision, P.A.F., A.S.S., and R.B. provided conceptual advice on the model and experiments and helped with the statistical analysis.

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684 **References Cited**

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- Rorsman, P., and F. M. Ashcroft. 2018. Pancreatic β-cell electrical activity and insulin
 secretion: Of mice and men. *Physiol. Rev.* 98:117-214.
- 688 2. Henquin, J. C. 2000. Triggering and amplifying pathways of regulation of insulin
 689 secretion by glucose. *Diabetes*. 49:1751-1760.
- Henquin, J. C. 1988. ATP-sensitive K⁺ channels may control glucose-induced electrical
 activity in pancreatic B-cells. *Biochem. Biophys. Res. Commun.* 156:769-775.
- Ashcroft, F. M., D. E. Harrison, and S. J. H. Ashcroft. 1984. Glucose induces closure of
 single potassium channels in isolated rat pancreatic β-cells. *Nature*. 312:446-448.
- 694 5. Cook, D. L., and N. Hales. 1984. Intracellular ATP directly blocks K⁺ channels in
 695 pancreatic B-cells *Nature*. 311:271-273.
- 696 6. Nunemaker, C. S., and L. S. Satin. 2014. Episodic hormone secretion: a comparison of
 697 the basis of pulsatile secretion of insulin and GnRH. *Endocrine*. 47:49-63.
- Satin, L. S., P. C. Butler, J. Ha, and A. S. Sherman. 2015. Pulsatile insulin secretion,
 impaired glucose tolerance and type 2 diabetes. *Mol. Aspects Med.* 42:61-77.
- 8. Bertram, R., L. S. Satin, and A. S. Sherman. 2018. Closing in on the mechanisms of
 pulsatile insulin secretion. *Diabetes*. 67:351-359.
- 702 9. Keizer, J., and G. Magnus. 1989. ATP-sensitive potassium channel and bursting in the
 703 pancreatic β cell. *Biophys. J.* 56:229-242.
- Magnus, G., and J. Keizer. 1998. Model of β-cell mitochondrial calcium handling and
 electrical activity. I. Cytoplasmic variables. *Am. J. Physiol.* 274:C1158-C1173.
- Detimary, P., P. Gilon, and J. C. Henquin. 1998. Interplay between cytoplasmic Ca²⁺ and
 the ATP/ADP ratio: a feedback control mechanism in mouse pancreatic islets. *Biochem*.
 J. 333:269-274.
- 709 12. Chen, L., K. Duk-Su, and B. Hille. 2003. Dynamics of calcium clearance in mouse
 710 pancreatic β-cells. *Diabetes*. 52:1723-1731.
- 711 13. Denton, R. M. 2009. Regulation of mitochondrial dehydrogenases by calcium ions.
 712 *Biochim. Biophys. Acta.* 1787:1309-1316.

713 14. Li, J., H. Y. Shuai, E. Gylfe, and A. Tengholm. 2013. Oscillations of sub-membrane ATP 714 in glucose-stimulated beta cells depend on negative feedback from Ca²⁺. *Diabetologia*. 715 56:1577-1586. 716 15. Merrins, M. J., C. Poudel, J. P. McKenna, J. Ha, A. Sherman, R. Bertram, and L. S. Satin. 717 2016. Phase analysis of metabolic oscillations and membrane potential in pancreatic islet 718 β cells. Biophys. J. 110:691-699. 719 16. Tsaneva-Atanasova, K., C. L. Zimliki, R. Bertram, and A. Sherman. 2006. Diffusion of 720 calcium and metabolites in pancreatic islets: Killing oscillations with a pitchfork. 721 Biophys. J. 90:3434-3446. 722 17. Ren, J., A. Sherman, R. Bertram, P. B. Goforth, C. S. Nunemaker, C. D. Waters, and L. 723 S. Satin. 2013. Slow oscillations of K_{ATP} conductance in mouse pancreatic islets provide 724 support for electrical bursting driven by metabolic oscillations. Am. J. Physiol. 305:E805-725 E817. 726 18. Pedersen, M. G., R. Bertram, and A. Sherman. 2005. Intra- and inter-islet 727 synchronization of metabolically driven insulin secretion. *Biophys. J.* 89:107-119. 19. 728 Sherman, A., J. Rinzel, and J. Keizer. 1988. Emergence of organized bursting in clusters 729 of pancreatic β-cells by channel sharing. *Biophys. J.* 54:411-425. Benninger, R. K. P., and D. J. Hodson. 2018. New understanding of β-cell heterogeneity 730 20. 731 and in situ islet function. Diabetes. 67:537-547. 732 21. Chay, T. R., and J. Keizer. 1983. Minimal model for membrane oscillations in the 733 pancreatic β-cell. *Biophys. J.* 42:181-190. 734 Fridlyand, L. E., N. Tamarina, and L. H. Philipson. 2003. Modeling of Ca²⁺ flux in 22. 735 pancreatic β-cells: role of the plasma membrane and intracellular stores. Am. J. Physiol. 736 285:E138-E154. 737 23. Fridlyand, L. E., D. A. Jacobson, A. Kuznetsov, and L. H. Philipson. 2009. A model of action potentials and fast Ca^{2+} dynamics in pancreatic β -cells. *Biophys. J.* 96:3126-3139. 738 739 24. Cha, C. Y., Y. Nakamura, Y. Himeno, J. Wang, S. Fujimoto, N. Inagaki, Y. E. Earm, and 740 A. Noma. 2011. Ionic mechanisms and Ca^{2+} dynamics underlying the glucose response of 741 pancreatic β cells: a simulation study. J. Gen. Physiol. 138:21-37. 742 25. Félix-Martínez, G. J., and J. R. Godínez-Fernández. 2014. Mathematical models of 743 electrical activity of the pancreatic β -cell: A physiological review. *Islets*. 6:3:e949195.

- Tantama, M., J. R. Martínez-François, R. Mongeon, and G. Yellen. 2013. Imaging energy
 status in live cells with a fluorescent biosensor of the intracellular ATP-to-ADP ratio. *Nat. Commun.* 4:2550.
- Partam, R., and A. Sherman. 2004. A calcium-based phantom bursting model for
 pancreatic islets. *Bull. Math. Biol.* 66:1313-1344.
- 28. Marinelli, I., V. Parekh, P. Fletcher, B. Thompson, J. Ren, X. Tang, T. L. Saunders, J.
- Ha, A. Sherman, R. Bertram, and L. S. Satin. 2022. Slow oscillations persist in pancreatic
 beta cells lacking phosphofructokinase M. *Biophys. J.* 121:692-704.
- Fridlyand, L. E., L. Ma, and L. H. Philipson. 2005. Adenine nucleotide regulation in
 pancreatic β-cells: modeling of ATP/ADP-Ca²⁺ interactions. *Am. J. Physiol.* 289:E839E848.
- Nunemaker, C. S., R. Bertram, A. Sherman, K. Tsaneva-Atanasova, C. R. Daniel, and L.
 S. Satin. 2006. Glucose modulates [Ca²⁺]_i oscillations in pancreatic islets via ionic and
 glycolytic mechanisms. *Biophys. J.* 91:2082-2096.
- Ashcroft, S. J. H., L. C. C. Weerasinghe, and P. J. Randle. 1973. Interrelationship of islet
 metabolism, adenosine triphosphate content and insulin release. *Biochem. J.* 132:223231.
- Gembal, M., P. Gilon, and J. C. Henquin. 1992. Evidence that glucose can control insulin
 release independently from its action on ATP-sensitive K⁺ channels in mouse β cells. *J. Clin. Invest.* 89:1288-1295.
- Rinzel, J., and Y. S. Lee. 1987. Dissection of a model for neuronal parabolic bursting. *J. Math. Biol.* 25:653-675.
- Rinzel, J., and G. B. Ermentrout. 1998. Analysis of neural excitability and oscillations. In
 Methods in Neuronal Modeling: From Synapse to Networks. C. Koch, and I. Segev,
 editors. MIT Press, Cambridge.
- Fridlyand, L. E., N. Tamarina, and L. H. Philipson. 2010. Bursting and calcium
 oscillations in pancreatic beta-cells: specific pacemakers for specific mechanisms. *Am. J. Physiol.* 299:E517-532.
- 772 36. Göpel, S. O., T. Kanno, S. Barg, L. Eliasson, J. Galvanovskis, E. Renström, and P.
- 773 Rorsman. 1999. Activation of Ca^{2+} -dependent K⁺ channels contributes to rhythmic firing
- of action potentials in mouse pancreatic β cell. J. Gen. Physiol. 114:759-769.

775 37. Goel, P., and A. Sherman. 2009. The geometry of bursting in the dual oscillator model of 776 pancreatic β-cells. SIAM J. Appl. Dyn. Syst. 8:1664-1693. 777 38. Lewandowski, S. L., R. L. Cardone, H. R. Foster, T. Ho, E. Potapenko, C. Poudel, H. R. 778 VanDeusen, T. C. Alves, X. Zhao, M. E. Capozzi, I. Jahan, C. S. Nunemaker, J. E. 779 Campbell, C. J. Thomas, R. G. Kibbey, and M. J. Merrins. 2020. Pyruvate kinase controls 780 signal strength in the insulin secretory pathway. Cell Metab. 32:736-750. 781 39. Tarasov, A. I., F. Semplici, M. A. Ravier, E. A. Bellomo, T. J. Pullen, P. Gilon, I. Sekler, R. Rizzuto, and G. A. Rutter. 2012. The mitochondrial Ca²⁺ uniporter MCU is essential 782 783 for glucose-induced ATP increases in pancreatic β-cells. *PLoS One*. 7(7):e39722. 784 40. Haythorne, E., M. Rohm, M. van de Bunt, M. F. Brereton, A. I. Tarasov, T. S. Blacker, 785 G. Sachse, M. S. dos Santos, R. T. Exposito, S. Davis, O. Baba, R. Fischer, M. R. Duchen, P. Rorsman, J. I. MacRae, and F. M. Ashcroft. 2019. Diabetes causes marked 786 787 inhibition of mitochondrial metabolism in pancreatic β-cells. *Nature Comm.* 10:2474. 788 41. Himmel, D. M., and T. R. Chay. 1987. Theoretical studies on the electrical activity of 789 pancreatic β-cells as a function of glucose. *Biophys. J.* 51:89-107. 790 42. Atwater, I., C. M. Dawson, A. Scott, G. Eddlestone, and E. Rojas. 1980. The nature of 791 the oscillatory behaviour in electrical activity for pancreatic β -cell. In Biochemistry, 792 Biophysics of the Pancreatic β-Cell. Verlag, New York, pp. 100-107. 793 43. Nunemaker, C. S., M. Zhang, D. H. Wasserman, O. P. McGuiness, A. C. Powers, R. 794 Bertram, A. Sherman, and L. S. Satin. 2005. Individual mice can be distinguished by the 795 period of their islet calcium oscillations. *Diabetes*. 54:3517-3522. 796 44. McKenna, J. P., and R. Bertram. 2018. Fast-slow analysis of the integrated oscillator 797 model for pancreatic β-cells. J. Theor. Biol. 457:1520162. 798